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4 **Title** Isolation of Circulating Fetal Trophoblasts using Inertial Microfluidics for Non-
5 Invasive Prenatal Testing

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33

34 **Abstract**

35 While non-invasive prenatal testing based on cell-free fetal DNA (cffDNA) has recently

36 revolutionized the field of aneuploidy screening in pregnancy, it remains limited to aneuploidy

37 and microdeletion screening and is unable to reliably detect single gene disorders. A number

38 of recent studies have demonstrated the potential of circulating trophoblastic cells in providing

39 cell-based non-invasive diagnosis with sequencing or array-based assays. However,

40 considering the extreme rarity of these cells in blood, efficient, high-throughput and clinically

41 applicable enrichment technologies are yet to be developed.

1 This study demonstrates for the first time the utility of inertial microfluidics for efficient
2 isolation of trophoblastic cells from maternal peripheral blood. Under optimal operating
3 conditions, high-recovery yields (79%) were obtained using a trophoblastic cell-line, which
4 was subsequently confirmed with analysis of maternal blood. Feasibility of obtaining a
5 diagnosis from cells isolated from a maternal sample was demonstrated in a case of confirmed
6 fetal Trisomy 21 in which six fetal cells were found in a 7mL blood sample using fluorescence
7 *in situ* hybridization. Finally, we demonstrate that trophoblastic cells isolated using inertial
8 microfluidics could be picked and subjected to a clinically validated sequencing assay, paving
9 the way for further validation of this technology and larger clinical studies.

10 **1. Introduction**

11 Invasive prenatal testing using techniques such as chorionic villus sampling (CVS) and
12 amniocentesis aims to confirm a diagnosis of chromosomal abnormality in high-risk
13 pregnancies as established by traditional combined first trimester screening with nuchal
14 translucency (NT) ultrasound and measurement of maternal serum analytes (free beta-hCG and
15 PAPP-A). The inherent risk of miscarriage involved with invasive techniques and the high false
16 positive rate of traditional first trimester screening has been a significant barrier to widespread
17 application of prenatal aneuploidy screening.^[1] The widespread uptake of non-invasive prenatal
18 testing (NIPT) using cell free fetal DNA (cffDNA) can be largely attributed to the vastly
19 improved screening parameters with a higher detection rate and a substantially lower false
20 positive rate than previous first trimester screening methods. The use of non-invasive prenatal
21 testing techniques has substantially reduced the number of invasive procedures and thus the
22 inherent risks of population-level screening, including patients with low-risk pregnancies.

23 The discovery of circulating cell-free fetal DNA (cffDNA) in 1997^[2] offered access to the fetal
24 genome without the risks of invasive testing, and the improved throughput of sequencing
25 technologies using next generation sequencing (NGS) has established the clinical validity of

1 non-invasive testing for aneuploidy screening and a limited range of monogenic disorders.
2 Currently, there are a number of commercial NIPT technologies clinically available to screen
3 for common fetal aneuploidies (e.g. Illumina Verifi™ and Harmony™) through the analysis of
4 cffDNA in maternal blood.^[3] Although cffDNA NIPT has revolutionized aneuploidy screening
5 in obstetric practice, there are a number of inherent limitations of the technique when
6 considering the full range of genetic disorders encountered in prenatal diagnosis. First,
7 although recent studies have shown that the whole fetal genome is present in the maternal
8 circulation, distinguishing between the fetal genome and the background maternal genome is
9 not possible, and only limited coverage of the fetal genome can be achieved reliably using
10 current protocols. NIPT allows for the reliable detection of the common aneuploidies at high
11 sensitivity ($\geq 99\%$ for trisomy 21, $\geq 92\%$ for trisomy 18, and $\geq 87\%$ for trisomy 13) and
12 specificity ($\geq 99\%$ for trisomy 21, 18, and 13), even for low risk pregnancies.^[4] Broader
13 applications of the technique for common microdeletions, genome wide screening, copy
14 number variants^[5], single gene disorders^[6] and X linked disorders have recently been developed
15 but these screening tests are characterized by significantly lower positive predictive values.
16 Thus, expansion of the NIPT testing portfolio to a wider array of conditions recreates the initial
17 problematic conditions of traditional first trimester screening in which patients were subjected
18 to invasive testing at much higher rates.

19 Circulating nucleic acids can be analyzed at higher genomic coverage but this is to likely
20 remain prohibitively expensive, does not overcome the problem of maternal cell-free DNA
21 background contamination^[7] and requires complicated bioinformatics.^[8] For example cffDNA
22 from a pregnant woman could be sequenced to a depth of 195× which provided a high positive
23 predictive value and could detect fetal *de novo* mutations (including BRAF which encodes a
24 proto-oncogene). The cost of sequencing at such a high depth is prohibitively expensive for
25 clinical translation even with the continuously decreasing sequencing cost.^[9] It is noteworthy

1 that, at this stage, and in the foreseeable future, cffDNA based NIPT is likely to remain only a
2 screening technology and clinical decision-making should be carried out only after
3 confirmation of the findings by diagnosis from fetal cells obtained by invasive testing. It is also
4 important to note that since NIPT has been introduced, it has drastically decreased the number
5 of invasive procedures. As a result, due to the current limited diagnostic capacity of cffDNA
6 this has led to a decreased diagnostic yield and hence delayed diagnosis in about 1 in 350 cases.
7 ^[10]

8 Access to a whole uncontaminated fetal genome from a non-invasive blood sample would
9 undoubtedly vastly improve the performance of NIPT. The fact that fetal cells are shed from
10 the developing placenta and circulate in maternal blood has been known for over a century.^[11]
11 To this end, the isolation of intact fetal cells from the maternal circulation is potentially
12 advantageous over cffDNA approaches as it likely will allow for more comprehensive genetic
13 analysis in a more cost-effective manner and could potentially eliminate the need for invasive
14 approaches. However, until recently NIPT based on circulating fetal cells has been a tantalizing
15 yet frustrating goal due to their extremely low number in maternal blood. Extremely efficient
16 enrichment technologies are required to isolate intact fetal cells from maternal blood with the
17 level of purity required for reliably conducting diagnostic assays. Fetal cell isolation methods
18 should be rapid, accurate and inexpensive in order to be truly useful in a clinical setting.^[12]
19 Techniques include density gradient centrifugation, fluorescence activated cell sorting (FACS),
20 magnetic activated cell sorting (MACS)^[13] and filtration, which all have been used with
21 moderate success to isolate fetal cells in the laboratory environment.^[13] However, these
22 technologies are typically time- and resource-intensive and have significant drawbacks
23 including low isolation efficiencies and low specificities. Consequently, they have failed to
24 provide a valid alternative to the current invasive antenatal testing approaches in the clinical
25 environment.

1 A small number of successful cases of fetal cell isolation and subsequent genetic analysis with
2 detection of genetic abnormalities including aneuploidy, microduplication and structural
3 rearrangements have been recently reported and brought a renewed vigor to the fetal cell-based
4 NIPT field.^[14, 15] In most recent studies after an initial enrichment step, the enriched cell
5 fraction is spread on a slide and automated microscopy coupled with laser capture
6 microdissection or micropipette aspiration is used to obtain single fetal cell. The performance
7 of the initial enrichment step is critical as high levels of fetal cell recovery/WBC depletion
8 would allow for better clinical scalability and therefore relevance.^[16] The reliance on laser
9 capture microdissection to obtain the fetal cells adds significant complexity, cost and scalability
10 issues to such processes thus hindering the translation into clinics. There is therefore, a
11 significant need to develop technologies able to isolate circulating fetal cells from biological
12 fluids in a high throughput fashion and to deliver these cells in a format readily compatible
13 with modern genomic approaches. With these requirements in mind, we endeavored to
14 demonstrate the feasibility of isolating circulating trophoblastic cells using inertial
15 microfluidics.

16 Circulating extravillous trophoblasts are fetal cells of placental origin which occur early in
17 pregnancy (from 5 weeks gestation) and with dimensions typically larger than white blood cells
18 (WBCs) ($>15\ \mu\text{m}$).^[17] The number of circulating trophoblasts in maternal blood is estimated to
19 be $\sim 1\text{-}5$ trophoblasts^[15] per mL of blood, although this is believed to vary with gestation^[17],
20 sex^[18] as well as with pregnancy conditions^[19] and genetic abnormalities.^[20] Importantly,
21 extravillous trophoblasts are not found post-termination/birth.^[17] Syncytial nuclear aggregates
22 (SNA) have also been consistently observed in maternal blood. SNAs are large fragments of
23 the outer layer of the placenta, the syncytiotrophoblast, which is formed by the fusion of
24 progenitor cytotrophoblasts into a continuous cell layer. Increased SNA number is observed in
25 pregnancy complications including preeclampsia^[21], reduced fetal movement, intrauterine

1 growth restriction^[22] and stillbirth when compared to healthy pregnancies.^[23] The large size of
2 trophoblastic cells and SNAs provides a mechanism for isolation which has previously been
3 exploited by the Isolation by Size of Epithelial Tumor/Trophoblast cells (ISET) test, a filtration
4 system developed by RARECELLS for maternal blood. This test provided 100% diagnostic
5 sensitivity and specificity in 63 pregnancies between 9 and 11 weeks of gestation at risk for
6 cystic fibrosis or spinal muscular atrophy.^[17] However, the ISET is very labor intensive as it
7 relies on laser capture microdissection of the isolated fetal cells among a background of WBCs,
8 and despite these promising results, has not been translated clinically.

9 Recent technological advances in rare cell isolation from peripheral blood have been driven by
10 the interest in isolating circulating tumor cells (CTCs) as a source of non-invasive molecular
11 information about solid malignancies.^[24] Cell separation technologies based on the concept of
12 inertial microfluidics have been one of the very few approaches successfully translated
13 clinically for the enrichment of CTCs based on size and deformation.^[25, 26] CTCs are indeed
14 generally larger than WBCs, a feature that is exploited in inertial microfluidics to achieve
15 efficient yet high-throughput separation.^[27-29]

16 The slanted inertial microfluidic devices used in this study have been modified from the
17 previously reported slanted inertial microfluidic CTC enrichment device.^[27, 28] A key
18 characteristic of the slanted design is the ability to efficiently process large volumes of blood
19 (>20ml), which is especially important in the context of circulating fetal cells as their number
20 in a normal pregnancy is extraordinary small. **Figure 1** is a schematic representation of the
21 experimental approach used in this study. Under optimal operating conditions, trophoblastic
22 cells could be enriched from blood within minutes and with high efficiency, delivering the
23 enriched population in the form of a cell suspension with small (<0.5%) WBC contamination.
24 The enriched cell fractions can be easily analyzed using a range of downstream methods. In

1 this study, we demonstrate successful diagnosis of fetal trisomy 21 using fluorescence *in situ*
2 hybridization (FISH) with automated laser scanning cytometry. Finally, we demonstrate the
3 feasibility of performing testing using a clinically validated sequencing approach from single
4 trophoblastic cells isolated using inertial microfluidics.

5 **2. Results**

6 2.1 Feasibility Study with a Trophoblastic Cell Line

7 In order to demonstrate the feasibility of using inertial microfluidic technology for the
8 enrichment of circulating trophoblastic cells and optimize the operating parameters, a
9 trophoblastic cell line was used (JEG3 choriocarcinoma cell line). Fluorescently labeled
10 trophoblastic cells were spiked into blood collected from healthy donors which was
11 subsequently lysed and processed through the inertial microfluidic device. Under optimal
12 operating conditions, a recovery rate of 79% (n=6) was determined using imaging flow
13 cytometry (**Figure 2**). In this instance, 1000 JEG3 cells were spiked per mL of blood. Although
14 this number of cells exceeds the expected circulating fetal cell load in healthy maternal blood,
15 it provides better accuracy of the enrichment yield as manipulating ultra-small cell numbers
16 is challenging and inherently associated with fairly large deviation. However, in order to better
17 simulate a real sample, we have subsequently investigated spiking ~30 JEG cells per mL of
18 blood in a total of 4 mL (n=4). We found that with this low number we maintained a high
19 recovery determined with microscopy of approximately 75%. The larger breast
20 adenocarcinoma cell line MCF-7 was also tested and a recovery of 91% was obtained (data not
21 shown), in agreement with previous CTC studies.^[28, 29]

22 Detailed analyses indicated that the lower recovery obtained for the JEG3 cells (vs MCF-7) is
23 primarily due to the significant cell size variation present in this cell line. Indeed, imaging flow
24 cytometry was used to quantify the dimensions of the JEG3 cells present in both enriched and
25 WBC/waste outlets and as presented in **Figure 3**, the area (Figure 3A), height, length and width

1 (Figure 3B) of the JEG3 cells found in the waste outlet were lower than those measured for
2 cells in the enriched outlet. Although only limited information is available about the
3 dimensional characteristics of circulating fetal trophoblastic cells present in the maternal
4 circulation, the size heterogeneity of JEG3 cells makes them a suitable surrogate which
5 provides a realistic mimic of the recovery of heterogeneous trophoblastic cells from maternal
6 blood.

7 Along with the recovery yield, the depletion of blood cells is the other essential performance
8 indicator. WBC depletion rates of 99.5% were consistently obtained using different donors and
9 operators. In a normal hematocrit, such a depletion rate will result in approximately 10,000
10 WBC/mL of blood present in the enriched outlet. Besides the performance of the device, the
11 processing time is also an important consideration, especially in the context of fetal
12 trophoblastic cells which are likely apoptotic and have been reported to be very fragile. Under
13 the optimal operating conditions, the equivalent of a 10mL blood tube could be processed
14 within 45 min (including RBC lysis, centrifugation and running of the inertial microfluidic
15 device).

16 2.2 Pilot Study with a Trisomy 21 Pregnancy

17 After having optimized the inertial microfluidic devices using a trophoblastic cell line, we
18 aimed to demonstrate the feasibility of obtaining a prenatal diagnosis through cytological
19 testing of circulating trophoblastic cells isolated using inertial microfluidics. For this purpose,
20 a blood sample from a woman carrying a fetus at high risk for Trisomy 21 was obtained from
21 the Maternal Fetal Medicine unit at the Women's and Children's Hospital (Adelaide, South
22 Australia). The blood sample was obtained at 11 weeks gestation and the fetus was
23 subsequently confirmed as being affected with Trisomy 21 using amniocentesis and
24 karyotyping.

1 To demonstrate the presence of circulating fetal cells in the sample, this maternal blood was
2 first processed with the inertial microfluidic device, and the enriched cellular population
3 stained with cytokeratin, CD45 and DAPI and analyzed with imaging flow cytometry.
4 Cytokeratins, especially Cytokeratin 7 and 8, are known to be expressed in placental cells and,
5 although it is not specific, are the most widely used markers for circulating trophoblastic
6 cells.^[30, 31] These analyses revealed the presence of 4 cytokeratin positive cellular events (from
7 7 mL whole blood) (**Figure 4**). We also observed the presence of white blood cells in at least
8 one of these clusters (cluster 3 in Figure 4) which could be an artefact induced during the
9 sample processing or a specific interaction between the circulating trophoblastic cells and
10 WBC in the peripheral circulation. Cytokeratin has been shown to be expressed in 76% of
11 extravillous trophoblasts (isolated by MACS specific for CD105) in maternal circulation^[32] so
12 it is possible that more fetal cells were present in this sample. No cytokeratin positive
13 cells/clusters were found in the blood of healthy donors used as a control. Morphological
14 analysis of cytokeratin positive events showed these cells were clustered and/or multinucleated
15 and thus suggestive of SNAs (Figure 4). On average, positive events had an area of 321
16 μm^2 (min 168, max 468), an average length of 27.2 μm (min 16.5, max 37.5) and width of 18.7
17 μm (min 14, max 26) (**Table 1**). It has been reported that syncytiotrophoblast fragments from
18 uterine venous blood vary from 20-200 μm and contain between 2-100 nuclei which are
19 normally densely packed, pyknotic with abundant heterochromatin and are often tear shaped,
20 while cytotrophoblasts are often found in cytokeratin positive clusters.^[33] Moreover,
21 trophoblasts in peripheral blood have similar characteristics and syncytial fragments normally
22 range between 100-200 μm with approximately 30 nuclei.^[34] Other characteristics of
23 trophoblasts include multinucleated (12-14 μm), diploid (7 μm) or nucleated cell remnants (5
24 μm).^[34] Cytotrophoblasts have been reported with diameters varying 11-14 μm and 19-25
25 μm .^[35] In this study the inertial microfluidic device used is designed to recover cellular

1 structures greater than approximately 15 μm and therefore, we expect that clustered and/or
2 large multinucleated cells would be separated in a similar manner as large mononucleated
3 cytotrophoblast cells. Smaller trophoblasts including nucleated cell remnants might therefore
4 not be efficiently enriched.

5 Next, we demonstrated the feasibility of using chromosomal FISH combined with laser
6 scanning cytometry to obtain a diagnosis from the isolated circulating trophoblastic cells. Fetal
7 cells were considered positive when the nuclei had two green signals for Chromosome 13 and
8 three red signals for Chromosome 21. Under the gating conditions, events were excluded if two
9 or more nuclei were in contact (i.e. two nuclei touching was excluded from analysis as this will
10 display as one event with >4 signals Chromosome 21). Therefore, only single cytotrophoblast
11 cells (not multinucleated SNAs) could be detected with this semi-automated algorithm. From
12 the 7ml blood sample that was tested with FISH, 6 cells with three red signals for 21
13 chromosome were detected (**Figure 5**). This result is in agreement with the expected
14 occurrence of such circulating fetal trophoblastic cells in maternal blood and confirmed the
15 feasibility of obtaining a diagnostic result using the combination of inertial microfluidics and
16 FISH. Note, however, when automatically scanning FISH slides it can be difficult to maintain
17 plane of focus and defective hybridization can occur resulting in missing true positive cells.^[20]
18 It has also been shown that as fetal cells are very fragile, 15% are lost during the FISH process,
19 and 9% could not undergo FISH.^[31] It is likely that the approach used here underestimates the
20 number of circulating trophoblastic cells present in the tested blood sample.

21 2.3. Feasibility Study of Performing Single Fetal Cell Sequencing

22 In order to determine the feasibility of inertial microfluidics as an initial enrichment step before
23 genomic studies JEG3 cells were spiked into whole blood as described previously. JEG3 cells
24 were retrieved from the enriched fraction and single cells were amplified, sequenced, aligned
25 to the human genome and chromosome copy number determined. This study demonstrated

1 successful isolation of single JEG3 cells which were able to be sequenced and chromosome
2 copy number determined using Veriseq and MiSeq technology (Illumina) **Figure 6** presents
3 typical profiles of a normal male cell from a healthy donor (Figure 6A) and a trophoblastic
4 hypertriploid JEG3 cell (Figure 6B).

5 **3. Discussion**

6 A number of recent studies have shown the feasibility of performing diagnostic genomic testing
7 on fetal cells isolated from maternal blood.^[14, 15, 30, 36] Considering the extremely low number
8 of these cells in the blood circulation, a prerequisite requirement is the application of an ultra-
9 efficient enrichment technology. Enrichment facilitates and fastens the detection, and therefore
10 the collection of the placental cells of fetal origin among the background maternal WBCs. It
11 also reduces the occurrence of false positives. In most contemporary approaches, the enriched
12 sample is placed on slides and scanned for the target cells which are then subsequently
13 collected, for example using laser capture microdissection or micropipette aspiration.

14 Magnetic activated cell sorting (MACS) is commonly used to enrich target cells based on either
15 specific surface expression^[14] (CD141 and CD105 are common^[18, 31, 32]) on the fetal cell
16 (positive enrichment) or specific surface expression on the WBCs (negative enrichment).

17 Under optimal conditions, MACS provides good WBC depletion (~120,000 residual WBCs
18 from 30 ml of blood).^[14] Arcedi BioTech has developed a panel of specific fetal antibodies for
19 fetal trophoblastic cell enrichment with MACS and has been shown to recover on average 12.8
20 fetal cells per 30 mL. These cells could be subsequently successfully used for whole genome
21 amplification and aCGH.^[15] However, blood processing (30 mL) with MACS separation
22 subsequent staining and spreading takes up to 7 hours and the total process blood sampling to
23 fetal cell picking takes up to 15 hours.^[14]

24 Density gradient centrifugation is also commonly used in the enrichment of fetal cells.
25 However, it does not provide a high enrichment, can damage cells and is associated with

1 significant cell loss.^[12, 37] In one instance it was reported that density gradient centrifugation
2 resulted in the loss of 60-80% of the fetal cells and that the procedure resulted in cellular
3 degradation^[37], therefore, it was recommended to improve upon this, that aggressive
4 manipulations should be eliminated and different gradients (other than Histopaque 1.119g/ml)
5 and densities should be tested to minimize cell loss. Combining density gradient with a negative
6 enrichment technique such as RosetteSep™ with antibodies such as anti-CD45 and/or anti-
7 CD36 to crosslink and cause the sedimentation of WBC can vastly decrease maternal cell
8 contamination.^[30] The enriched trophoblasts from 30 mL of blood could then be recovered and
9 retrieved with a semi-automated single cell retrieval device and could be subjected to whole
10 genome amplification and a-CGH or next-generation sequencing (NGS). However, the use of
11 this enrichment was shown to decrease the number of trophoblastic cells recovered from 0.74
12 to 0.36 per ml of blood^[30] and CD45 depletion has also been responsible for complete loss of
13 fetal cells.^[38]

14 We demonstrate for the first time the use of inertial microfluidics for the enrichment of
15 circulating fetal trophoblastic cells from the maternal circulation. The performance and clinical
16 relevance of inertial microfluidics for the isolation of CTCs is now well established.^[28, 29] A
17 commercial instrument, the ClearCell® FX1 system from Clearbridge BioMedics, has already
18 received CE marking. The high throughput, nature of inertial microfluidics, makes it ideal to
19 analyze large volumes of blood, separating physically larger cells i.e. fetal trophoblastic cells
20 from smaller surrounding blood cells. A high recovery yield (>75%) was obtained using the
21 JEG3 trophoblastic cell line as a model, even for very low cell numbers (30 cells /mL) used to
22 better mimic the clinical situation. Inertial microfluidics allows for fast enrichment, with the
23 time from obtaining the blood to an enriched sample being acquired being less than 45min for
24 20ml of blood. Because of the known fragility of circulating trophoblastic cells, it is preferable
25 to either process samples quickly or fix them prior to the enrichment step.^[31] Fixation before

1 pre-enrichment with MACS can be applied, however, this resulted in clogging of the columns
2 in 13% of cases.^[31] Beside its relatively low processing time, a significant advantage of inertial
3 microfluidics is that it is very gentle on the target cells, as shown with CTCs.^[26]

4 We also demonstrated the feasibility of establishing a diagnostic technique using circulating
5 trophoblastic cells isolated using inertial microfluidics. Six circulating fetal cells could be
6 enriched from a 7 mL blood sample obtained from a Trisomy-21 affected pregnancy. It is
7 noteworthy that the presence of genetic abnormalities (particularly Trisomy 21) has been
8 previously reported to be associated with an increase in the number of trophoblastic cells.^[20, 23]

9 Early pioneering work using the ISET filtration system illustrated the potential of size-based
10 enrichment of circulating trophoblastic cells. ISET could indeed be applied to detect spinal
11 muscular atrophy in a number of fetuses.^[17] Despite early promising results, the technical
12 limitations of this system, including the reliance on laser capture microdissection which can be
13 cumbersome and time consuming requiring an experienced user^[12], has to date prevented its
14 clinical implementation. A new approach has been recently reported based on the Nano-Velcro
15 microchips initially developed for the capture of CTCs.^[18] After an initial pre-enrichment step
16 with density gradient centrifugation, the sample is injected in a microfluidic device presenting
17 a PLGA roughened nanosubstrate functionalized with an anti-epithelial cell adhesion molecule
18 (EpCAM). However, the technique takes over 5 hours to enrich the fetal cells and 2 hours to
19 isolate cells within the chip itself for 2 mL of blood meaning it is very time consuming for such
20 a low throughput (especially when compared to the high throughput nature of inertial
21 microfluidics). Once attached to the device surface cells are laser capture micro-dissected with
22 3 cells pooled for whole genome amplification followed by microarray analysis.^[39]

23 While the majority of the research in the field of cell-based NIPT has been devoted to blood,
24 trophoblastic cells can also be obtained from the endocervical canal. Although this route
25 provides a likely lesser challenge than the isolation of fetal cell from blood considering the

1 larger number of trophoblastic cells present in the endocervical canal, high levels of enrichment
2 is still required to allow for clinical translation. Samples from the endocervical canal have been
3 recently used successfully to isolate^[40] and perform NGS for genomic profiling from 5 weeks
4 gestation.^[41] Enrichment was performed using HLA-G MACS and testing was performed using
5 whole genome/exome sequencing to identify chromosomal structural abnormalities and *de*
6 *novo* mutations.^[18] However, the patient acceptability of this approach is likely lower with
7 comparison to peripheral blood sampling. Nevertheless, inertial microfluidics could be readily
8 applied to enrich samples obtained from the endocervical canal although its performance in
9 this setting remains to be determined.

10 Finally, an important consideration in the development of a circulating fetal enrichment
11 technology is its compatibility with the downstream strategy used to test for the presence of
12 genetic abnormalities. Technologies including RT-PCR, chromosomal FISH, whole genome
13 sequencing and array comparative genomic hybridization (aCGH) have been used in the
14 literature.^[13, 17, 32, 42] Sequencing-based diagnostic testing is likely to be broadly clinically
15 implemented in the near future and recent progress in the field allows for testing to be carried
16 out from very small number of cells down to the single cell level. Indeed recent studies have
17 demonstrated advanced genetic analysis for circulating fetal cells including aCGH and single
18 cell NGS which have demonstrated copy number differences for whole and sub-chromosomal
19 aberrations^[14] and deep sequencing towards screening for monogenic disorders.^[36]

20 To demonstrate the feasibility of inertial microfluidics with sequencing-based testing, we
21 developed a methodology to pick-up single fetal trophoblastic cells. To this end, the enriched
22 sample was stained for cytokeratin (KRT), CD45 and DAPI and automated microscopy was
23 used to identify the trophoblastic cells. We have also shown that cells that have been processed
24 with this method can be used to carry out genetic testing, and in this case we have used the

1 Veriseq protocol used for preimplantation genetic screening approach utilizing Illumina MiSeq
2 which can determine chromosomal copy number. Although in this instance the NGS profile
3 was noisy which may be influenced by stage of cell cycle or cell degradation it must be noted
4 that sample aligned to the human genome with >350,000 reads and due to the fact that
5 chromosome Y was detected indicates JEG3 cells were successfully isolated, amplified and
6 sequenced from a female spiked blood sample.

7 **3. Conclusion**

8 The data presented in this study demonstrates that inertial microfluidics provides an efficient
9 yet simple and gentle method to isolate rare fetal cells from maternal blood. Although this
10 approach should be validated in a clinical study, inertial microfluidics possesses many
11 advantages over standard enrichment approaches towards the isolation of circulating fetal
12 cytotrophoblast and SNA as has been demonstrated in this feasibility study from maternal
13 blood at 11 weeks gestation. Most notably, inertial microfluidic technology provides high
14 throughput, rapid and gentle isolation that is not reliant on antibody expression. We have also
15 shown that inertial microfluidics separation is amenable to downstream genetic analysis with
16 a commercially available single cell preimplantation genetic screening approach.

17 The development and validation of a clinical technology for the efficient isolation of circulating
18 fetal trophoblasts would foster the development of novel truly non-invasive prenatal test, with
19 a strong potential to improve on the emerging gold standard method based on cffDNA
20 including elimination of the maternal contribution which can influence current NIPT
21 technology. Further development of this technology could not only eliminate the risks
22 associated with current invasive procedures, but also provide reassurance to the large majority
23 of low risk pregnancies.

24 **4. Experimental Section**

1 *Characterization of Inertial Microfluidics*

2 To optimize and enable accurate detection of the enrichment yields, MCF-7 breast cancer cell
3 lines and JEG3 a Human choriocarcinoma cell line (ECACC) stained with calcein (Sigma
4 Aldrich, St. Louis, MO., USA) were used to mimic large trophoblastic cells. The cancer cell
5 lines was cultured in 25 or 75cm² tissue culture flasks (Sarstedt, Nümbrecht Germany) in
6 DMEM or AMEM supplemented with fetal bovine serum and penicillin/streptomycin (Sigma
7 Aldrich, St. Louis, MO., USA) at 37°C, 5% CO₂ in a humidified environment. Cancer cells
8 were detached from culture flasks with trypsin/EDTA (Sigma Aldrich, St. Louis, MO., USA)
9 and spiked into healthy blood samples. Healthy peripheral blood was collected from volunteers
10 (in compliance with the University of South Australia Human Research Ethics Committee) into
11 an EDTA vacutainer, and used within 24 hours after collection. Cell preparation and isolation
12 were performed as outlined in the following sections. Cell recovery was quantitated with
13 imaging flow cytometry based on the recovery of calcein positive events (cancer cells) and
14 calcein negative events (WBC).

15 *Sample Collection and Ethical Considerations*

16 Ethics approval for sample collection (maternal peripheral blood) was approved by the
17 Women's and Children's Human Research Ethics committee (WCH Application No:
18 WEC/13/WCHN 45). Written informed consent was obtained from the patient prior to sample
19 collection. It is important to note patients were enrolled in this study before undergoing
20 amniocentesis, and that these patients are at an increased risk of genetic abnormalities.
21 Maternal peripheral blood (14 mL) sample was taken just before amniocentesis (at
22 approximately 11 weeks' gestation), by a trained nurse and was placed into K3EDTA
23 Vacutainers and kept on ice or at 4°C until use. All samples were processed within 6 hours after
24 collection. To eliminate epithelial contamination commonly seen in blood drawn by
25 venipuncture, the first 2ml will be discarded. Healthy peripheral blood samples were collected

1 from healthy donors in compliance with the University of South Australia Human Research
2 Ethics Committee.

3 *Cell Preparation and Isolation*

4 Chemical red blood cell lysis was performed at room temperature with a 1:10-1:25 blood to
5 lysis solution (145mM NH₄Cl, 10mM KHCO₃, 0.1mM EDTA in MilliQ water; Sigma Aldrich)
6 dilution. After 10 minutes of shaking, samples were centrifuged at 500g for 10 minutes, the
7 cell pellet was then washed and resuspended in PBS (×2 dilution) and the cellular suspension
8 was loaded in a syringe. From this point inertial microfluidics was used to further enrich the
9 fetal cells obtained from the maternal sample. The suspension was then injected through tygon
10 tubing with a syringe pump into the inertial microfluidic chips (1700 μL/min) using a standard
11 syringe pump (KD Scientific Legato Syringe pump). Eluted suspension, enriched in
12 trophoblastic cells, were then collected and processed for downstream analyses. The
13 microfluidic chips was fabricated using micromilling at the SA and NSW nodes of the
14 Australian National Fabrication Facility with each being subjected to a strict control quality
15 protocol.

16 *Fluorescence Staining and Imaging Flow Cytometry*

17 For use with the imaging flow cytometer cells were stained with the nuclear stain DAPI (4',6-
18 diamidino-2-phenylindole) and with fluorescently labelled fluorochromes Anti-Human CD45
19 PE-Cy5.5 or Alexa 488 and Anti-Pan-Cytokeratin (AE1/AE3) Alexa Fluor® 488 or 660
20 (eBioscience, San Diego, CA, USA) using a standard flow cytometry protocol previously
21 described.^[43] Imaging flow cytometry was performed using the ImageStream^x Mark II
22 (AMNIS, Seattle, WA, USA) and analysis of the cellular population was performed with
23 IDEAS software Version 6.1 (AMNIS, Seattle, WA, USA). Potential trophoblast cells were
24 identified as DAPI positive, CD45 negative with cytokeratin staining. Events per sample were

1 acquired at 40× magnification. 3 healthy blood samples from non-pregnant women was also
2 run to confirm there was no false positive KRT staining.

3 *Fluorescence in situ Hybridization (FISH) and Laser Scanning Cytometry*

4 A maternal blood sample from a pregnancy with Trisomy 21 was processed and the large cells
5 were isolated with inertial microfluidics as described above (7 mL whole blood processed for
6 FISH protocol). The trophoblast outlet sample was resuspended in hypotonic solution
7 (0.05mol/L potassium chloride) and left at room temperature for 10 minutes. Carnoy's fixative
8 (3:1 methanol/acetic acid) was then added to the sample and centrifuged at 1100 rpm for 5
9 minutes. Supernatant was removed and cells were resuspended completely in Carnoy's
10 fixative. This was repeated twice more and the sample was then stored at 4°C in Carnoy's
11 fixative until further processing. After centrifugation again Carnoy's fixative was removed
12 leaving behind approx. 100 µl total volume, cells were resuspended in this volume and then
13 spread onto slides. Slides were left to air dry before probes (spectrum green, 21 spectrum
14 orange, AneuVysion Multicolor DNA probe kit) were applied to the slide and a coverslip
15 placed on top and sealed with rubber cement to avoid drying out. Samples were hybridized at
16 75°C for 5 minutes, before being incubated at 30°C overnight. Slides were washed with 0.4×
17 Saline-sodium citrate buffer (SSC) with NP-40 (pH 7) at 75°C for 2 minutes and then with
18 2xSSC with NP-40 (pH 7) for 1 minute. Slides were mounted with DAPI anti-fade (Vector
19 Shield) and a cover slip added for imaging. Microscopy was carried out using the CompuCyte
20 iCys™ Laser Scanning Cytometer using DAPI (blue), FITC (green) and Cy3/PE (red) channels
21 for detection of nuclei, Chromosome 13 and Chromosome 21, respectively. Using the software
22 and a compucolour6 filter DAPI positive events with three 21 signals were identified. Positive
23 cells had three distinct and separate 21 chromosome signals inside the nucleus with a similar
24 intensity. A sample from a male pregnancy and also a healthy sample from a non-pregnant

1 women were also run following the procedure as described above with 0 false positive events
2 found.

3 *Cell Retrieval and Genetic Analysis*

4 As with characterization of inertial microfluidics JEG3 cell lines (XY-male) have been spiked
5 into a healthy blood sample (XX-female). Sample is then enriched with inertial microfluidics,
6 fixed with formalin, stained for KRT, CD45 and DAPI as per fluorescence staining method.
7 Sample is then injected into a well with a thin PBS layer and oil on top as previously
8 described.^[44] KRT positive and CD45 negative cell well is then scanned with a Nikon TiE
9 fluorescence microscope and KRT positive, CD45 negative events were identified and
10 retrieved manually with a Celsorter (Celsorter Company for Innovations, Budapest,
11 Hungary). Individual cells are placed into a 2µl of PBS (Cell Signaling Technology,
12 Massachusetts, USA) and stored at -80°C until sequencing was undertaken. Briefly the cell
13 sample was amplified using the Sureplex DNA Amplification kit (Illumina) which utilizes
14 linker-adaptor PCR technology. Cells were lysed and extracted using lysis buffer and extraction
15 buffer/enzyme. This was followed by pre-amplification and amplification as per manufacturer
16 instructions. All temperature incubation steps were performed on a thermo-cycler (Simpliamp,
17 Life Technologies, Thermofisher). For each round of amplification a positive female DNA
18 control (15 pg genomic DNA in 2.5 µl 1x PBS) was used and the negative control was equal
19 to 2.5 µl of PBS. Confirmation of amplification was determined on agarose gel using the E-
20 Gel@iBase™system (Invitrogen, Thermofisher). Following this chromosome copy number
21 was determined using sequencing by synthesis technology (Veriseq, Illumina) which uses
22 paired-end dual index sequencing on a Miseq (Illumina). Reads were aligned to the human
23 genome and chromosome copy number status was determined using Bluefuse Multi software
24 (Illumina).^[45]

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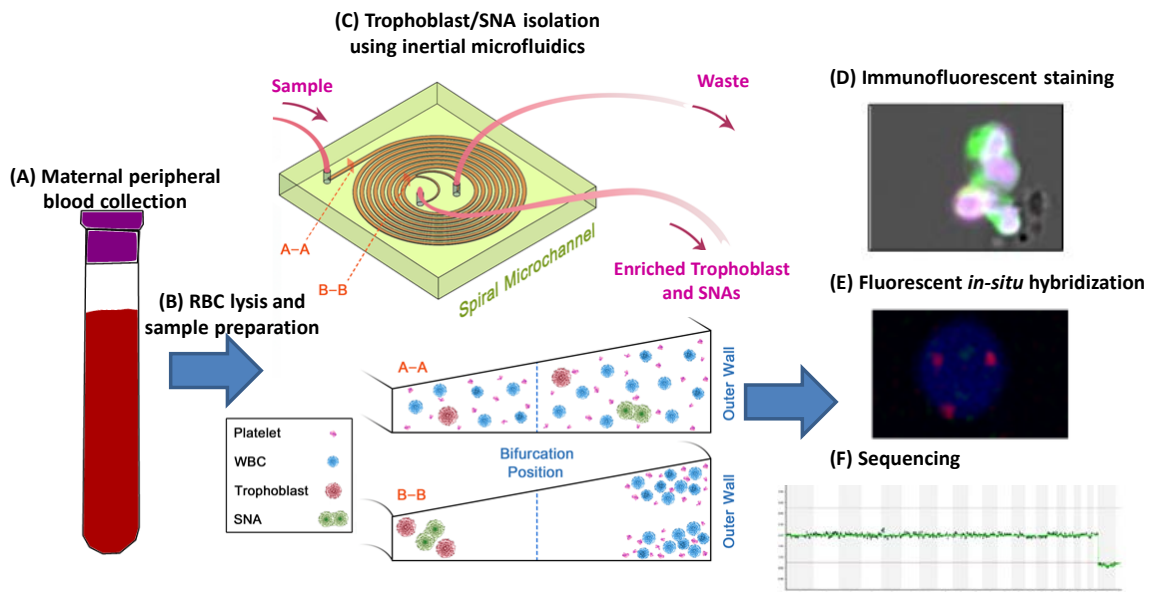
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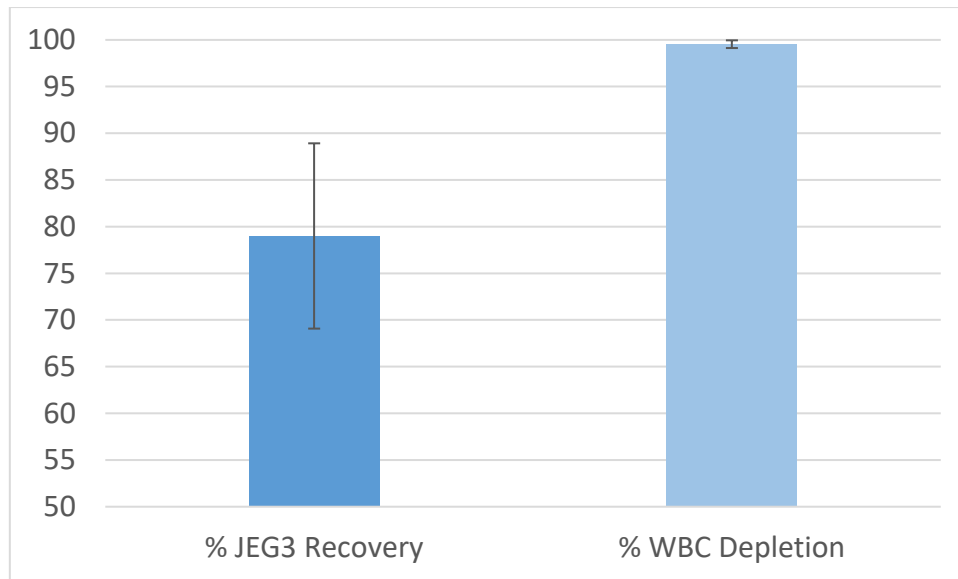
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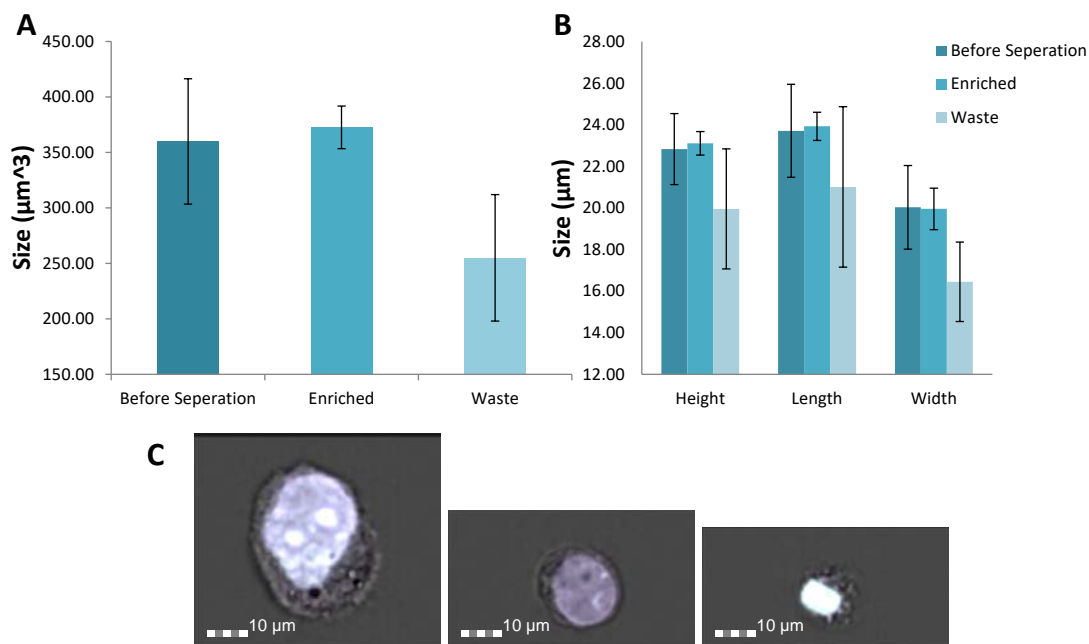
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Figure 1 Schematic diagram of the experimental protocol followed when analyzing maternal blood for isolation and staining of fetal cells A) Maternal blood was collected and processed within 6 hours. B) Red blood cells were lysed and C) the nucleated cell fraction (nucleated fetal cells; white blood cell, WBC) was collected and resuspended in phosphate buffered saline (PBS). Samples were run through the inertial microfluidic device using a syringe pump at 1700 μ l/min. D) Trophoblast (inner) outlet was plated and stained with CD45, KRT (cytokeratin) and DAPI and imaged with imaging flow cytometry. E) Fluorescence *in situ* hybridization (FISH) was performed on the trophoblast outlet and imaged with a standard fluorescence microscope or Laser Scanning Cytometry. F) Example of a normal male cell isolated with this method and sequenced as a model of a trophoblastic cell.



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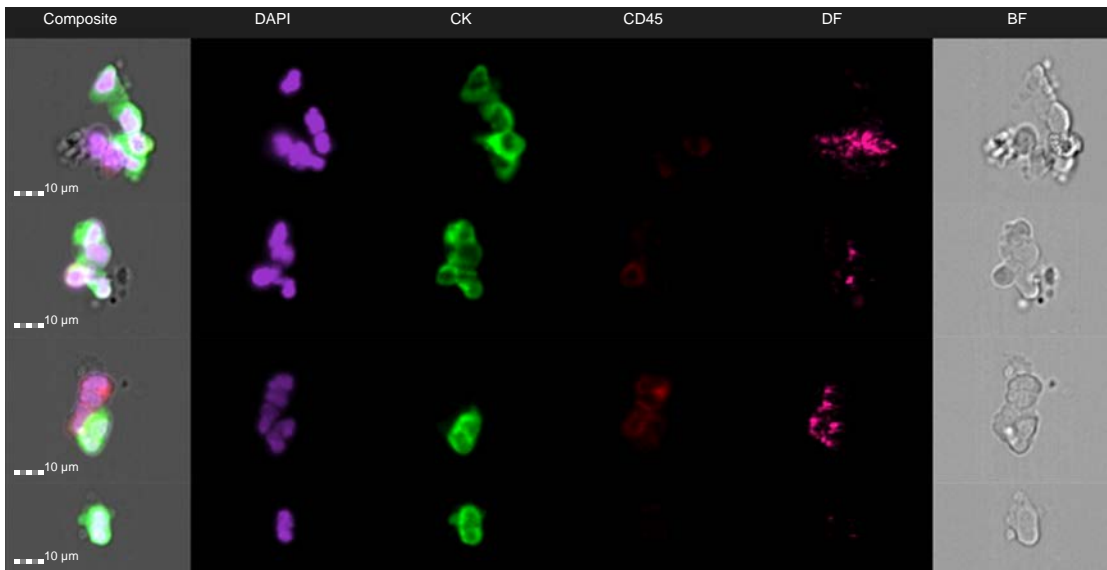
Figure 2 Bar graph depicting the recovery percent of JEG3 cells after inertial microfluidic enrichment and percent white blood cell (WBC) depletion of the enriched outlet after passing through the inertial microfluidics.



6

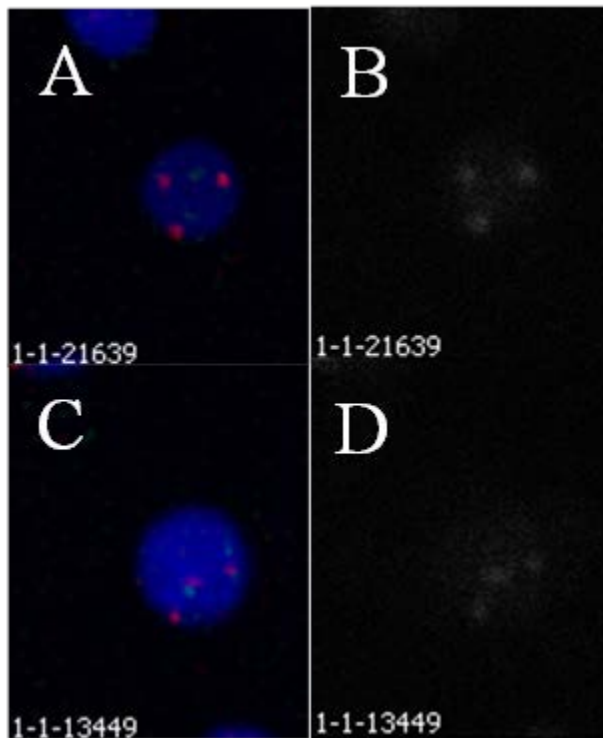
Figure 3 JEG3 size characteristics based on brightfield from the imaging flow cytometer with cells from before separation with inertial microfluidics or recovered after separation from the big cell or white blood cell (WBC) outlets. A) Graph of single cell area, B) Graph of single cell height, length and width. C) Imaging flow cytometry micrographs (composite image with brightfield and nuclei stained with Hoechst) of JEG3 cells demonstrating their large size variation.

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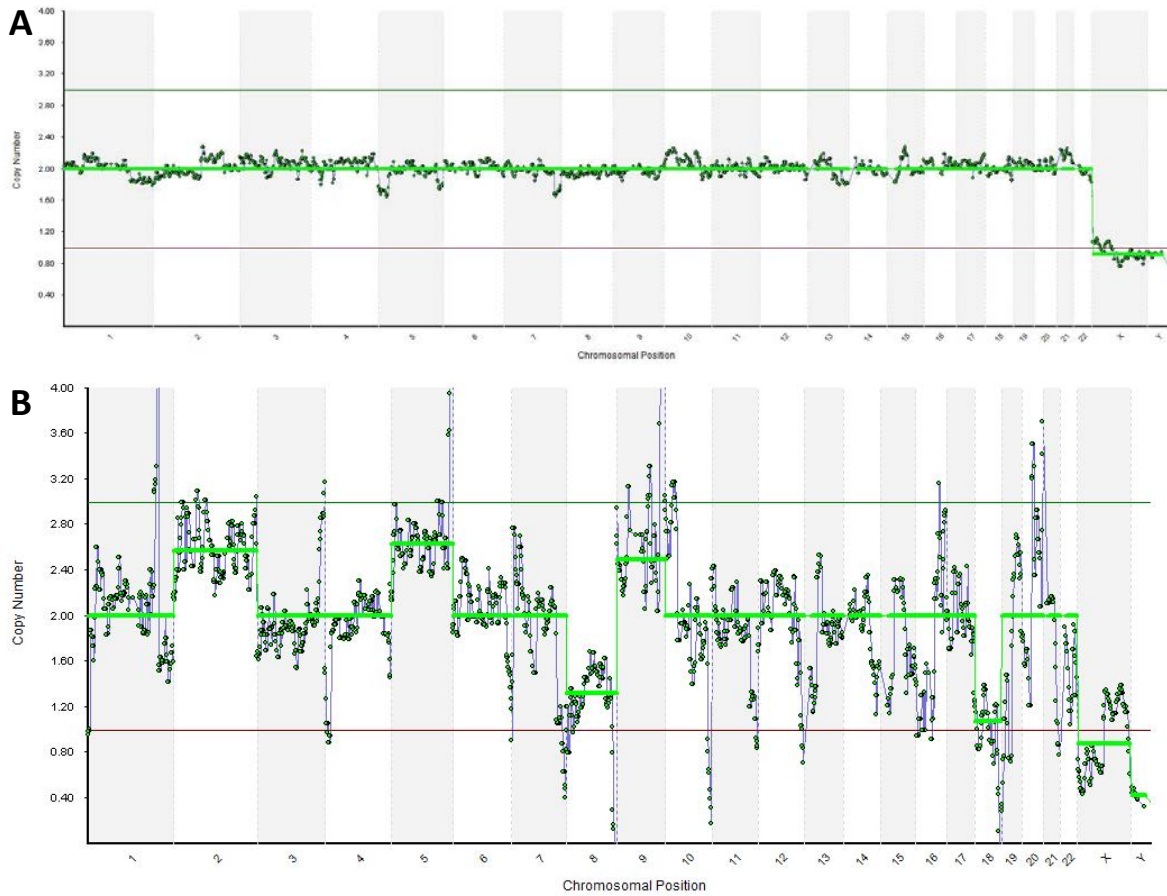
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2 **Figure 4** Trophoblastic images of cytokeratin positive events from the imaging flow cytometer
 3 from a maternal blood sample (Trisomy 21) that has undergone inertial microfluidic
 4 enrichment. Images have been adjusted to enhance visual appearance and were all taken at
 5 40×magnification.



6

7 **Figure 5** Fetal cells positive for Trisomy 21 (chromosome 21; red signal, and chromosome 13;
 8 green signal) identified from a maternal blood sample carrying a male fetus with diagnosed
 9 Trisomy 21 abnormality. A, C) Processed computed color image of fetal cells and B, D) raw
 10 fluorescent red signal.



1
 2 Figure 6 Individual cells are placed in a PCR tube and undergo sequencing with Illumina
 3 MiSeq. Profile from individual normal male cell (A) and an abnormal JEG3 cell hypertriploid
 4 profile (B).

5
 6
 7 **Table 1.** Cytokeratin Positive Trophoblast Characteristics from Trisomy 21 affected
 8 pregnancy

	Average	St Dev	Min	Max
Area (μm^2)	321	150	168	468
Length (μm)	27.2	10.5	16.5	37.5
Width (μm)	18.7	6.43	14	26

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