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Hyperspectral microscopy can detect metabolic heterogeneity within bovine post-compaction embryos incubated under two oxygen concentrations (7% versus 20%)

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1 **Title: Hyperspectral microscopy can detect metabolic heterogeneity within**
2 **bovine post-compaction embryos incubated under two oxygen**
3 **concentrations (7% versus 20%)**

4

5 **Running Title:** Metabolic heterogeneity in embryos

6

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27 **Abstract**

28 **Study Question:**

29 Can we separate embryos cultured under either 7% or 20% oxygen atmospheres
30 by measuring their metabolic heterogeneity?

31

32 **Summary Answer:**

33 Metabolic heterogeneity and changes in metabolic profiles in morula exposed to
34 two different oxygen concentrations were not detectable using traditional
35 fluorophore and two-channel autofluorescence but were detectable using
36 hyperspectral microscopy.

37

38 **What is Known Already:**

39 Increased genetic and morphological blastomere heterogeneity is associated with
40 compromised developmental competence of embryos and currently forms the
41 basis for embryo scoring within the clinic. However, there remains uncertainty
42 over the accuracy of current techniques, such as PGS and time-lapse microscopy,
43 to predict subsequent pregnancy establishment.

44

45 **Study Design, Size, Duration:**

46 The impact of two oxygen concentrations (7% = optimal and 20% = stressed)
47 during post-fertilisation embryo culture was assessed. Cattle embryos were
48 exposed to the different oxygen concentrations for 8 days (D8; embryo
49 developmental competence) or 5 days (D5; metabolism measurements). Between
50 3-4 experimental replicates were performed, with 40-50 embryos per replicate

51 used for the developmental competency experiment, 10-20 embryos per replicate
52 for the fluorophore and two-channel autofluorescence experiments and a total of
53 21-22 embryos used for the hyperspectral microscopy study.

54

55 **Participants/Materials, Setting, Methods:**

56 In-vitro produced (IVP) cattle embryos were utilised for this study. Post
57 fertilisation, embryos were exposed to 7% or 20% oxygen. To determine impact
58 of oxygen concentrations on embryo viability, blastocyst development was
59 assessed on D8. On D5, metabolic heterogeneity was assessed in morula (on-time)
60 embryos using fluorophores probes (active mitochondria, hydrogen peroxide and
61 reduced glutathione), two-channel autofluorescence (FAD and NAD(P)H) and 18-
62 channel hyperspectral microscopy.

63

64 **Main Results and the Role of Chance:**

65 Exposure to 20% oxygen following fertilisation significantly reduced total
66 blastocyst, expanded and hatched blastocyst rates by 1.4-, 1.9- and 2.8-fold
67 respectively compared to 7% oxygen ($P < 0.05$), demonstrating that atmospheric
68 oxygen was a viable model for studying mild metabolic stress. The metabolic
69 profiles of D5 embryos was determined and although metabolic heterogeneity
70 was evident within the cleavage stage (i.e. arrested) embryos exposed to
71 fluorophores, there were no detectable difference in fluorescence intensity and
72 pattern localisation in morula exposed to the two different oxygen concentrations
73 ($P > 0.05$). While there were no significant differences in two-channel
74 autofluorescent profiles of morula exposed to 7% and 20% oxygen (main effect, P
75 > 0.05), morula that subsequently progressed to the blastocyst stage had

76 significantly higher levels of FAD and NAD(P)H fluorescence compared to arrested
77 morula ($P < 0.05$), with no change in the redox ratio. Hyperspectral
78 autofluorescence imaging (in 18-spectral channels) of the D5 morula revealed
79 highly significant differences in four features of the metabolic profiles of morula
80 exposed to the two different oxygen concentrations ($P < 0.001$). These four
81 features were weighted and their linear combination revealed clear
82 discrimination between the two treatment groups.

83

84 **Limitations, Reasons for Caution:**

85 Metabolic profiles were assessed at a single time point (morula), and as such
86 further investigation is required to determine if differences in hyperspectral
87 signatures can be detected in pre-compaction embryos and oocytes, using both
88 cattle and subsequently human models. Furthermore, embryo transfers should be
89 performed to determine the relationship between metabolic profiles and
90 pregnancy success.

91

92 **Wider Implications of the Findings:**

93 Advanced autofluorescence imaging techniques, such as hyperspectral
94 microscopy, may provide clinics with additional tools to improve the assessment
95 of embryos prior to transfer.

96

97 **Study Funding/Competing Interest(s):**

98 This study was funded by the Australian Research Council Centre of Excellence for
99 Nanoscale BioPhotonics (CE140100003). The Fluoview FV10i confocal
100 microscope was purchased as part of the Sensing Technologies for Advanced

101 Reproductive Research (STARR) facility, funded by the South Australian Premier's
102 Science and Research Fund. The authors declare there are no conflict of interest.

103

104 **Key Words:**

105 Embryo, Pre-implantation, Metabolism, Heterogeneity, Oxygen, Embryo Culture,

106 Autofluorescence, Hyperspectral Microscopy.

107 **INTRODUCTION**

108 Pre-implantation embryos respond to their surrounding environment and both
109 in-vivo and in-vitro environments can influence developmental outcomes, such as
110 implantation and ongoing pregnancy (reviewed by (Fleming, et al., 2015) Early
111 development prior to embryonic genomic activation and compaction (4-8 cell
112 stage in humans and the 8-cell stage in ruminants) is particularly sensitive to
113 environmental perturbations, partly because there is limited communication
114 between blastomeres within the pre-compaction embryo. Communication
115 between individual blastomeres begins with the initiation of connexion formation
116 (the building blocks of gap junctions), coinciding with polarisation and
117 compaction (Bloor, et al., 2002, Eckert, et al., 2004, Houghton, 2005).

118

119 Cellular morphological heterogeneity forms the basis of morphological embryo
120 grading in the clinic, with healthier embryos having no obvious morphological
121 heterogeneity (Gardner, et al., 2007). An increase in the appearance of blastomere
122 heterogeneity is associated with poor quality embryos (Brison, et al., 2014).

123

124 Another form of blastomere heterogeneity within human embryos is their
125 karyotype. The extent of chromosomal mosaicism within pre-compaction (Day 3)
126 human embryos is such that a single biopsied cell may not reflect accurately the
127 chromatin profile of the remaining blastomeres within an embryo (Voullaire, et
128 al., 2000, Wells and Delhanty, 2000). More accurate techniques of assessing
129 mosaicism within trophectoderm cells recovered by biopsy of blastocyst stage
130 embryos has revealed a greater incidence than first thought, and increased

131 mosaicism appears to be associated with a reduction in pregnancy rates (Munne
132 and Wells, 2017), although this association remains controversial (Gleicher, et al.,
133 2014).

134

135 There is a surge of interest from human IVF clinics to apply time-lapse microscopy
136 to predict embryo developmental outcomes. Time-lapse measures morphokinetic
137 parameters such as the timing of syngamy, periods between cytokinesis, and
138 oolema ruffling and abnormal cytokinetic events resulting in uneven blastomere
139 sizes (reviewed by (Wong, et al., 2013), as these parameters that may correlate
140 with embryo developmental outcomes (VerMilyea, et al., 2014). Nevertheless,
141 morphokinetic analysis over the first three days of development that predict
142 subsequent blastocyst development does not predict implantation (Chamayou, et
143 al., 2013).

144

145 A recent hypothesis (Brison, et al., 2014) connects increasing cellular stress with
146 increased blastomere metabolic heterogeneity. Measuring embryo metabolism is
147 viewed by many researchers as the cellular parameter most likely to reflect
148 embryo developmental outcomes (Thompson, et al., 2016). However, most of the
149 current methodologies measuring embryo metabolism cannot measure individual
150 blastomere metabolic heterogeneity. Non-invasive measurements of substrate
151 turnover in spent culture media using microfluorometric analyses or
152 spectrometer-based metabolomics (Krisher, et al., 2015) represent the metabolic
153 profile of the whole embryo, but not the metabolic variation between blastomeres.
154 Furthermore, such metabolic measurements are usually performed at a single
155 time point of development. Hence, alternative non-invasive technologies are

156 needed to measure individual blastomere metabolism, preferably in real-time and
157 throughout development. This should provide the clearest relationship between
158 blastomere metabolic variation and assessment of embryo stress, which is likely
159 to reflect developmental outcome.

160

161 Metabolic differences between oocytes and embryos can be determined
162 temporally and in real time using autofluorescence. Published examples include
163 examinations of metabolism during fertilization of mouse oocytes (Dumollard, et
164 al., 2004) or of the impact of recombinant oocyte secreted-factors on metabolism
165 of cattle cumulus-oocyte complexes (Sutton-McDowall, et al., 2012, Sutton-
166 McDowall, et al., 2015). Most studies involve two-channel excitation wavelengths,
167 specifically targeting the two metabolic cofactors, NAD(P)H and FAD. Recently,
168 we explored a broader spectral approach, hyperspectral imaging of embryo
169 autofluorescence, which involved up to 18 spectral channels. Autofluorescence
170 can be used to provide insights into metabolism, for example through separately
171 identified bound- and free-NADH and NADPH (e.g. Fluorescence Lifetime Imaging
172 Microscopy, Cinco et al 2016). Furthermore, our laboratory has explored the
173 utility of Grey Level Co-occurrence Matrices (GLCM) applied to embryo
174 autofluorescence, to increase the capacity for discrimination between different
175 treatments applied to embryos during development (Tan, et al., 2016). It has been
176 recently demonstrated that hyperspectral microscopy of cell autofluorescence
177 and features analysis with GLCM was able to distinguish biomolecular and
178 metabolic differences in cultured somatic cells and embryos (Gosnell, et al.,
179 2016a, Gosnell, et al., 2016b).

180

181 The oxygen concentration within the reproductive tract during development is
182 lower than in the atmosphere (Fischer and Bavister, 1993). Many studies across
183 several species demonstrate that low oxygen levels (typically 5-7%) for culture of
184 pre-implantation embryos improve developmental outcomes compared to
185 atmospheric levels (Thompson, et al., 1990, Thompson, 2000, Bontekoe, et al.,
186 2012, Guo, et al., 2014, Gardner, 2016). Relative to low oxygen levels, exposure to
187 atmospheric oxygen concentrations increases reactive oxygen species levels and
188 of oxidative damage, and both gene and protein expression profiles within
189 embryos reflect a greater degree of cellular stress (Wale and Gardner 2016).
190 Hence, exposure to a low oxygen concentration relative to atmosphere during
191 development was employed in this study as a model for inducing cellular stress.
192 We routinely utilize 7% O₂ for ruminant embryo culture, based on our previous
193 publication (Thompson, et al., 1990).

194

195 The aim of this study was to assess the metabolic heterogeneity of pre-
196 implantation cattle embryos cultured under 7% and 20% O₂ levels, with a view to
197 determine whether autofluorescence has potential for clinical assessment of
198 embryo development outcomes. Firstly, embryos were imaged using a
199 combination of fluorescence stains to assess blastomere heterogeneity between
200 the two treatments. This was followed by examination with two non-invasive
201 autofluorescence techniques by confocal microscopy examining two excitation
202 channels, and its extension, hyperspectral imaging, using bespoke 18 spectral
203 channels with varying excitation and emission bandwidths. Their data were,
204 respectively, analysed using GLCM and through combined features of colour and
205 morphology.

206

207 **MATERIALS AND METHODS**

208 Unless otherwise stated, all chemicals and reagents were purchased from Sigma
209 Aldrich.

210

211 **Oocyte and Embryo Culture**

212 Cattle ovaries were transported from a local abattoir in warm saline (30-35 °C)
213 and follicular contents were aspirated from 3-8 mm follicles using an 18-gauge
214 needle and a 10 ml syringe. The aspirate was allowed to settle and intact cumulus-
215 oocyte complexes (COCs) with greater than four cell layers of compact cumulus
216 and ungranulated ooplasm were selected in undiluted follicular fluid and washed
217 twice in IVM medium. IVM medium was VitroMat (IVF Vet Solutions, Adelaide
218 Australia) + 4 mg/ml fatty acid free (FAF) BSA (MP Biomedicals, Solon OH USA) +
219 0.1 IU/ml FSH (Puregon; Organon, Oss Netherland). Groups of 40-50 COCs were
220 transferred into 500 µl of pre-equilibrated IVM medium, overlaid with paraffin oil
221 and cultured for 23 h at 38.5°C, 6% CO₂ in humidified air.

222

223 At the completion of IVM, COCs were washed once in wash medium (VibroWash;
224 IVF Vet Solutions, + 4 mg/ml FAF BSA) and transferred into 500 µl of IVF medium
225 (VibroFert, IVF Vet Solutions; + 4 mg/ml FAF BSA + 10 IU/ml heparin + 25 µM
226 penicillamine + 12.5 µM hypotaurine + 1.25 µM epinephrine), overlaid with
227 paraffin oil. Two straws of bull sperm of proven fertility were thawed and
228 prepared using a discontinuous Percoll gradient (45%:90%; GE Healthcare) and

229 sperm were added to IVF wells at a final concentration of 1×10^6 sperm/ml. COCs
230 and sperm were co-cultured at 38.5°C, 6% CO₂ in humidified air.

231

232 After 23 h of COC and sperm co-culture (day 1; D1), presumptive zygotes were
233 mechanically denuded of cumulus cells by repeat pipetting in wash medium,
234 washed once in cleavage medium (VitroCleave, IVF Vet Solutions; + 4 mg/ml FAF
235 BSA) and five embryos were transferred into 20 µl drops of pre-equilibrated
236 cleavage medium, overlaid with paraffin oil. Presumptive zygotes were cultured
237 in 7% or 20% O₂, with 6% CO₂ in nitrogen balance at 38.5 °C.

238

239 On day 5 (D5), embryos were washed once in blastocyst medium (VitroBlast, IVF
240 Vet Solutions; + 4 mg/ml FAF BSA) and groups of five embryos were transferred
241 into 20 µl drops of pre-equilibrated blastocyst medium, overlaid with paraffin oil.
242 Embryos were cultured until day 8 (D8) in either 7% or 20 %O₂, with 6% CO₂ in
243 nitrogen balance at 38.5 °C.

244

245 **Developmental Competence of Embryos Following Culture at 7% or** 246 **20% O₂**

247 Embryo developmental stage was assessed on D8. In order to determine the
248 influence of different oxygen concentrations post-fertilisation on embryo quality,
249 four experimental replicates were performed with 40-50 COCs per treatment
250 within replicates.

251

252 **Anti-Oxidant, Reactive Oxygen Species and Mitochondrial Activity in**
253 **Day 5 Cleavage Stage Embryos and Morula**

254 On D5, embryos were classified as cleavage stage (delayed, pre-compaction) or
255 morula (on-time, post-compaction) and live embryos were co-stained with
256 peroxyfluor-1 (PF1), monochlorobimane (MCB) and Mitotracker Red CMXRos
257 (MTR, Invitrogen; Carlsbad CA, USA), as previously described (Sutton-McDowall,
258 et al., 2015). Briefly, PF1 is an aryl boronate probe that fluoresces on reaction with
259 hydrogen peroxide (H_2O_2), a reactive oxygen species (ROS) produced by
260 mitochondria; MCB fluoresces when bound to low weight thiol compounds, with
261 the highest affinity for reduced glutathione (GSH; representative of 99% of
262 fluorescence intensity; Keelan, et al., 2001), an anti-oxidant, and MTR is a
263 rosamine based fluorophore that accumulates within active mitochondria
264 (membrane potential dependent).

265

266 Embryos were washed and stained in wash media, beginning with a brief wash
267 and then each incubated at 38.5°C in semi-darkness with 20 μ M PF1 for 1 h, briefly
268 washed and moved into 12.5 μ M MCB for 30 m, briefly washed and then incubated
269 with 200 nM MTR for 15 m. Embryos were then washed once and transferred into
270 2 μ l drops of wash medium, and overlaid with paraffin oil, in glass bottomed
271 confocal dishes (Cell E&G, Houston TX, USA). Fluorescence was visualised using a
272 Fluoview FV10i (Olympus; Tokyo Japan) confocal microscopy (MCB: excitation =
273 358 nm and peak emission = 461 nm; PF1: excitation = 496 nm and peak emission
274 = 519 nm; MTR: excitation = 578 nm and peak emission = 598 nm) at 90x
275 magnification, at a single z plane. Laser settings, magnification and image settings
276 remained constant across replicates. Individual experimental runs were

277 normalised to fluorescence beads (InSpeck, Invitrogen) to account for any
278 variations in the instrument between runs.

279

280 Image processing and analysis of laser scanning confocal microscopy images was
281 performed using Image J software (NIH). Prior to analysis, images were converted
282 from Olympus image files (.oif) to 8-bit grey scale tiff images and positive staining
283 areas/region of interest (ROI) were selected using the threshold selection
284 function within ImageJ. The mean intensity and texture of the ROI was determined
285 using batch macros for intensity and grey-level co-occurrence matrix (GLCM),
286 both available online (<http://rsb.info.nih.gov/ij/plugins/index.html>) and as per
287 Sutton-McDowell et al. (Sutton-McDowall, et al., 2015).

288

289 Three texture feature analyses were conducted within the GLCM analysis.
290 “Orderliness” (predictability) of fluorescence is measured by angular secondary
291 moment (ASM), with increasing ASM values indicating more predictable patterns
292 and decreased heterogeneity. “Contrast” measures the variability in fluorescence
293 intensity as a broad measure of fluorescence homogeneity, with increasing values
294 indicating increased heterogeneity. “Correlation” relates to the linear dependence
295 of grey levels on neighbouring pixels (Haralick, et al., 1973), predictive of
296 organelle patterning.

297

298 Three experimental replicates were performed with 10-20 embryos per
299 treatment and developmental stage within each replicate.

300

301 **Redox State of Morula as a Predictor of Developmental Competence**

302 The autofluorescence (AF; NAD(P)H and FAD) of D5 morula embryos was
303 measured using laser scanning confocal microscopy to determine if there was a
304 relationship between redox state and embryo developmental potential. On D5,
305 morula-stage embryos cultured in 7% and 20% O₂ were washed once in wash
306 medium and transferred into individual 2 µl of wash medium in confocal dishes,
307 overlaid with mineral oil. Embryos (+AF) were imaged for NAD(P)H (excitation =
308 405 nm and emission = 420-520 nm) and FAD (excitation = 473 nm and emission
309 = 490-590 nm) using a Fluoview FV10i confocal microscope at 90x magnification
310 and at a single z plane. Embryos were washed once in blastocyst medium and then
311 transferred into 2 µl drops of blastocyst media and cultured individually. Control
312 embryos (without AF) were washed once in blastocyst medium and then
313 transferred into 2 µl drops of blastocyst medium. All embryos were cultured for a
314 further three days (D8) in either 7% or 20 %O₂, 6% CO₂ in nitrogen balance at
315 38.5 °C to assess whether the AF results on D5 (morula stage) correlated with
316 development to the blastocyst stage on D8. Small groups of embryos were imaged
317 per replicate (5-10 per dish per replicate, 4 replicates). Embryo handling in
318 atmosphere was limited to less than 10 mins during the image capture period to
319 minimise stress.

320

321 **Hyperspectral Analyses of Morula**

322 Day 5 embryos were air transported (3 h travel) to perform hyperspectral analysis
323 on live morula-stage embryos (7% O₂ = 21 embryos and 20% O₂ = 22 embryos),
324 as per previous publications (Gosnell, et al., 2016a, Gosnell, et al., 2016b). Briefly,

325 spectral autofluorescence was measured using an Olympus IX71 epifluorescent
326 microscope (Olympus), fitted with a multi LED light source (Prizmatix Ltd; Givat-
327 Shmuel, Israel). Hyperspectral microscopy utilises 18 spectral channels: 12
328 separate excitation wavelength ranges (generated by 12 different light emitting
329 diodes) and 4 emission wavelength bands, covering excitation wavelengths of
330 334-495 nm and emission wavelengths of 447-700 nm (see Table 1 for channel
331 details). Images were captured using an iXon 885 camera (Andor; Belfast, UK). The
332 power densities and exposures (~1 s) were comparable to standard fluorescence
333 microscopy (Gosnell, et al., 2016b). At these exposures, no detectable
334 photobleaching was observed.

335

336 Embryos were transferred into glass bottomed confocal dishes containing
337 cleavage medium and hyperspectral images were taken at five different z planes
338 in 10 µm increments, one image at the equatorial plane of focus of the embryo
339 (widest diameter), two images above and two images below. For each spectral
340 channel a composite, multi-focus image reconstruction was applied prior to
341 analysis (Gosnell, et al., 2016a, Gosnell, et al., 2016b).

342

343 **Hyperspectral Image Analysis**

344 Image analysis was performed as per Gosnell et al. (Gosnell, et al., 2016a, Gosnell,
345 et al., 2016b). Images containing cells were segmented to define a perimeter
346 around the cells' fluorescent cytoplasm. The boundaries of the fusing cells of
347 morula were manually segmented, based on the differential interference contrast
348 (DIC) images taken simultaneously with the hyperspectral images, creating
349 regions of interest (ROI) representing seemingly continuous areas (either single

350 blastomeres or very compacted blastomeres). The median value of the non-zero
351 pixels was subtracted from all non-zero pixels in order to greatly reduce the sharp
352 edge around the perimeter of the ROIs, whilst retaining most of the obvious
353 texture. Pixels within each ROI were used to calculate the features in each of these
354 cell regions.

355

356 Custom-designed software was used to determine multiple mathematically
357 defined cellular features, such as cell spectra, channel values and morphological
358 patterns (for the definition of features see Gosnell, et al., 2016b). A total of 33,000
359 feature algorithms were used in the analysis. Following feature selection process
360 and their ranking (carried out as in Gosnell, et al., 2016a), four such features were
361 identified to have strong correlation with embryo classes examined here (culture
362 at 7% or 20% O₂) and, taken together, they could demonstrate significant
363 differences between embryos cultured in the two O₂ concentrations. Descriptions
364 of the four features A-D are provided in the Supplementary Material.

365

366 **Colour Spectral Plots**

367 Autofluorescence data obtained in 18 channel hyperspectral imaging were
368 projected onto a three-dimensional space using Principal Component Analysis
369 with the top three PCA variables capturing most of the intensity variance. The
370 three new variables were then used to make false colour images
371 (red/green/blue), which are representative of spectral information in
372 autofluorescence. These false colour images are provided to highlight
373 differences of cellular biochemistry within the embryos.

374

375 **Statistical Analysis**

376 Differences between treatments were analysed using a general linear model using
377 version 22 (IBM) SPSS software, with oxygen concentrations built in as the main
378 effect. Embryo development data was arcsine transformed prior to analyses. Data
379 is presented as means \pm SEM and P-values less than 0.05 were considered
380 significant.

381

382 To analyse hyperspectral autofluorescence feature data, a discrimination plot was
383 created by performing linear discrimination analysis (LDA) of the four
384 hyperspectral features (selected out of 33,000 hyperspectral features). The linear
385 combinations of the best four features obtained by LDA most sensitively captured
386 the differences between 7% and 20% O₂ cultured embryos.

387

388 **RESULTS**

389 **Developmental Competence of Embryos Following Culture in 7% or** 390 **20% O₂**

391 From Day 1, putative zygotes were cultured in 7% or 20% O₂ and on-time embryo
392 development was determined on Day 8. There were no differences in cleavage
393 rates (Table 2). However, blastocyst development was significantly reduced, as
394 expected, following culture in 20% O₂ (Table 2, P < 0.05), particularly in advanced
395 stages of blastocyst development, with hatched blastocyst rates reduced 2.8-fold
396 in the presence of atmospheric oxygen levels (P < 0.05). Hence, the model for
397 embryo stress using low and high oxygen concentration was validated.

398

399 **Metabolic Heterogeneity in Day 5 Cleavage Stage Embryos and Morula**

400 The effects of 7% versus 20% oxygen concentration on reactive oxygen species
401 (ROS) production, anti-oxidants and mitochondrial activity within Day 5 embryos
402 was determined. In addition to measuring the mean fluorescence intensity,
403 texture analysis (grey level co-occurrence matrix; GLCM, examining three
404 features) was performed to predict the uniformity and frequency of the patterns
405 of fluorescence throughout the embryos.

406

407 Differences in colour from the merged fluorophore staining between morula and
408 arrested cleavage stage embryos was evident (Figure 1). The variability in the
409 merged fluorescence images between blastomeres within the cleavage stage
410 embryos demonstrated metabolic heterogeneity among blastomeres of arrested
411 cleavage stage embryos, whereas such visually clear heterogeneity was not
412 evident at the morula stage.

413

414 Only images of morula were used for subsequent analyses. The fluorescence
415 intensity of MCB (GSH) was significantly higher in embryos cultured in 20% O₂
416 compared to 7% O₂, (Table 3; 7% = 160.5 ± 3.8 vs. 20% = 173.4 ± 2.7 intensity
417 values; P = 0.007) and the 'predictability' (ASM) of fluorescence intensity patterns
418 was also higher in morula cultured in 20% O₂ (Table 3; ASM, a measure of
419 orderliness), with no significant differences in contrast and correlation
420 measurements of MCB fluorescence. The correlation (predictability of
421 fluorescence intensity at the pixel level) of PF1 fluorescence was also higher in
422 20% O₂ exposed embryos, compared to the 7% treatment group (Table 3; P <
423 0.001).

424

425 **Redox State of Morula as a Predictor of Metabolic Heterogeneity and**
426 **Developmental Outcome Following Autofluorescence Measurement**

427 To determine if conventional autofluorescence measurements by confocal
428 microscopy of morula (Day 5) was predictive of heterogeneity and embryo
429 developmental outcomes, FAD and NAD(P)H fluorescence were measured in
430 morula cultured in 7% or 20% O₂. Following measurement, morula were cultured
431 individually and the development was then assessed on Day 8 (Figure 2A). An
432 additional cohort of morula was removed from group culture into individual drops
433 to serve as a “no confocal microscopy” controls. Neither oxygen concentration
434 affected the number of morula that reached the blastocyst stage on Day 8 during
435 culture and fluorescence measurement (Table 4; main effects, $P > 0.05$),
436 suggesting that the positive impact of reduced oxygen was primarily during the
437 pre-compaction period of culture.

438

439 In contrast to the analysis with fluoroprobes, there were no significant
440 autofluorescence differences in intensity (and therefore redox ratio) or texture
441 between oxygen concentrations measured in Day 5 morula (data not shown, main
442 effect, $P > 0.05$). However, both FAD and NAD(P)H intensity were significantly
443 higher in Day 5 morula that developed to the blastocyst stage on Day 8, compared
444 to that in morula that arrested (Figure 2B and C; $P < 0.05$). There was no significant
445 differences in the redox ratio (Figure 2D, FAD:NAD(P)H), demonstrating that
446 increases in both FAD and NAD(P)H metabolism was predictive of further
447 development, suggesting that increased metabolic activity is associated with
448 advanced development in this model.

449

450 **Hyperspectral Analyses of Morula**

451 Colour spectral plots (composite two-dimensional images) were created to
452 highlight differences in cellular biochemistry, registered in all 18-hyperspectral
453 channels and z-stacks of five planes in which images were captured (Figure 3).
454 False Principle Component Analysis-derived colours were applied to the
455 hyperspectral image stacks as indicated in the Methods, with multiple hues within
456 embryos indicating enhanced variation in metabolic signatures. Representative
457 images are presented in Figure 3, with exposure to 20% O₂ resulting in morulae
458 with more hues (represented by Figure 3D-F) compared to morulae cultured in
459 7% O₂ where the hues were more uniform (represented by Figure 3A-C).

460

461 Furthermore, a suite of 33000 textural features was applied to the two-
462 dimensional z-stack reconstructions of embryo images. Of these, four features
463 revealed differences that were significantly different between morula exposed to
464 the different oxygen concentrations ($P < 0.001$; Figure 4). Morula cultured in the
465 presence of 7% O₂ had significantly higher mean log₁₀ intensity of the brightest
466 10% pixels in channel 5 (Excitation: 365 nm, Emission: 587 nm) compared to
467 morula exposed to 20% O₂ ($P < 0.001$; Figure 4A). Likewise, the standard
468 deviation of pixel intensity in channel 15 (Excitation: 495 nm, Emission: 587 nm)
469 was significantly higher in the 7% O₂ group compared to 20% O₂ (Figure 4D). The
470 other two features were significantly higher in the 20% O₂ treatment group.
471 Specifically, the “blobbiness” feature (indicative of increased disorderliness of
472 signal intensity) of channel 18 (Excitation: 495 nm, Emission: 635 nm) and the
473 mean intensity ratio of channel 11:channel 13 (Excitation: 425 nm, Emission: 587

474 nm and Excitation: 455 nm, Emission: 587 nm) were both significantly higher in
475 the 20% O₂ treatment (Figures 4B & C respectively; P < 0.001).

476

477 The values of the four features for each ROI in each embryo were then linearly
478 transformed using Linear Discrimination Analysis (LDA) with respect to the two
479 groups (7% O₂ and 20% O₂). A clear discrimination between the 7% and 20% O₂
480 treatment groups was apparent, with significant differences in the mean values of
481 clusters (Figure 5; P < 0.001).

482

483 **Discussion**

484 We employed a well-characterised model of cell stress (7% O₂ vs 20% O₂) in a
485 bovine embryo model to evaluate techniques that may quantify responses to
486 cellular stress. The ruminant embryo is exquisitely sensitive to oxygen levels
487 during culture (Tervit, et al., 1972, Thompson, et al., 1990). Our results clearly
488 support the observations of others that low oxygen culture reduces cell stress and
489 enhances pre-implantation development during in-vitro culture and therefore
490 should be the preferred atmosphere for human embryo culture (Katz-Jaffe, et al.,
491 2005, Rinaudo, et al., 2006, Gardner and Wale, 2013, Gardner, 2016).

492

493 We also employed fluorescent probes to target specific aspects of cellular
494 metabolism to observe whether embryo culture under either 7% or 20% oxygen
495 atmospheres induced different levels of metabolic heterogeneity in either
496 arrested (pre-compaction, cleavage stage) or embryos that had developed 'on-
497 time' (post-compaction, morula). It was visually evident that metabolic

498 heterogeneity is present in the arrested embryos (Figure 1). In extreme cases,
499 blastomeres within the same embryo that appear morphologically similar (shape,
500 size, density) under phase contrast microscopy had obvious variations in the
501 intensity of fluorescence. As expected, using the same fluorophore probes at the
502 morula stage revealed fewer differences in intensity and patterns in fluorescence
503 between the two culture conditions (as determined by texture analysis). We
504 would expect less heterogeneity at this stage of development, due to the
505 establishment of cell-cell communication. Nevertheless, GLCM analysis revealed
506 that MCB fluorescence was more consistent (predictable) when embryos were
507 cultured under 20% O₂ compared to 7% O₂. MCB fluorescence is specific for
508 reduced thiols, of which glutathione (GSH) is the most abundant. While increased
509 developmental competence in oocytes is correlated with increased levels of
510 reduced glutathione (de Matos and Furnus, 2000), it might also be associated with
511 a response to increased stress (Zeng, et al., 2014).

512

513 Autofluorescence of somatic cells has previously been shown to measure
514 differences in redox state, as the strongest fluorescence signals are derived from
515 the autofluorescence of NAD(P)H (Excitation: 405 nm and Emission: 420-520 nm)
516 and FAD (Excitation: 473 nm and Emission: 490-590 nm) (Skala and Ramanujam,
517 2010). Two-channel autofluorescence measurement has been used for
518 distinguishing differences in redox activity in oocytes and embryos as a result of
519 fertilisation and cleavage (Dumollard, et al., 2007a, Dumollard, et al., 2007b), and
520 the impact of different culture environments for oocyte in-vitro maturation and
521 early development (Zeng, et al., 2014, Sutton-McDowall, et al., 2015, Sutton-
522 McDowall, et al., 2016). Two-channel autofluorescence measurements were

523 applied at the morula stage to embryos cultured under 7% and 20% O₂
524 concentrations but neither autofluorescence channel was able to discriminate a
525 difference between the two culture conditions. However, higher levels of
526 autofluorescence were associated with the ability of morula to develop to the
527 blastocyst stage, which may have a clinical application as an embryo diagnostic
528 tool.

529

530 Four image analysis features were able to discriminate differences in
531 hyperspectral images of embryos cultured under either 7% or 20% oxygen. Unlike
532 the two-channel autofluorescence measurements, the more detailed 18 channel
533 hyperspectral microscopy and more sophisticated textural analysis was sensitive
534 enough to detect differences between morula exposed the two different culture
535 conditions. Hyperspectral autofluorescence analysis has been shown to
536 successfully separate differences between somatic cells in monolayer cultures,
537 demonstrating that cellular heterogeneity exists in large populations of cells
538 (Gosnell, et al., 2016a, Gosnell, et al., 2016b). Further studies are needed to
539 determine if differences can be seen in earlier stages of development, such as pre-
540 compaction, zygotes or oocytes, which could incorporate additional features
541 beyond the four that were used in the current study. In addition, further studies
542 are required in animals, then feasibly in IVF clinics, to evaluate the utility of
543 hyperspectral analysis by examining its predictive capacity for post-transfer
544 pregnancy establishment, which was logistically impossible to conduct in the
545 current study. Nevertheless, the data presented here describes an important new
546 tool to discriminate two populations of embryos that are difficult to separate on
547 morphology and less detailed metabolic measures alone. This approach to

548 discriminate between embryos may be an adjunct tool to combine with other
549 diagnostic methods to provide accurate embryo viability assessment.

550

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557

558 **Authors' Roles**

559 M.S.M. and J.T. conceived the idea for the study and experimental design; M.S.M.
560 and M.W. conducted the embryology, fluorophore and two-channel
561 autofluorescence experiments; M.P. and A.D.A. synthesised and developed the PF1
562 fluorophore; M.G., A.A. and E.G. conducted the hyperspectral microscopy and
563 subsequent analysis. M.S.M. wrote the initial draft of the manuscript, with all
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565

566

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573

574 **Conflict of Interest**

575 The authors declare no conflict of interest.

576

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733
734

735 **Figure Legends**

736 **Figure 1.** Representative images of Day 5 arrested (cleaved) and on-time (morula)
737 embryos cultured in 7% and 20% O₂ and labeled with fluorescence probes. MCB
738 = monochlorobimane (reduced glutathione); PF1 = perfluoxy 1 (hydrogen
739 peroxide) and MTR = Mitotracker Red CMXRos (active mitochondria). The scale
740 bar represents 50 μm.

741

742 **Figure 2.** Autofluorescence (AF) measured on a laser scanning confocal
743 microscope in two channels (representative of FAD and NAD(P)H) of morula (M)
744 on day 5, in relation to embryo developmental stage on day 8. A) Experimental
745 design; B) FAD; C) NAD(P)H and D) redox ratio (FAD:NAD(P)H). Dot plots indicate
746 individual embryos, with bars representing mean units \pm SEM. UnBl = unexpanded
747 blastocyst; ExBl = expanded blastocyst and HBl = hatched blastocyst. Asterisks
748 indicate significant differences to the morula group ($P < 0.05$).

749

750 **Figure 3.** Representative images of composite two-dimensional reconstructions
751 of the 90 images (5 z-planes and 18 spectral channels) of each morula. False
752 colours produced from the top three components in Principal Component Analysis
753 (PCA) indicate variability in metabolic signatures, with an increased number of
754 hues in a single embryo relating to increased heterogeneity. A-C = 7% O₂ and D-E
755 = 20% O₂.

756

757 **Figure 4.** Hyperspectral signatures of day 5 morula exposed to 7% or 20% O₂.
758 Feature values are A) the log₁₀ of the mean pixel intensity of the brightest 10%
759 pixels in channel 5 (Ex: 365nm, Em: 587nm; $P < 0.000026$); B) blobbiness feature
760 (measuring how well pronounced are various irregular oval shapes) in channel 18
761 (Ex: 495 nm, Em: 635 nm; $P < 0.00003$); C) mean cellular pixel intensity ratio of
762 channel 11:channel 13 (Ex: 415nm, Em: 587 nm vs. Ex: 455 nm, Em: 587nm; P
763 $< 1e-06$) and D) standard deviation of pixel intensity of channel 15 (Ex: 495 nm,
764 Em: 587 nm; $P < 0.000084$). Dot plots represent individual regions of interests and
765 the bars with shading represent mean \pm SEM.

766

767 **Figure 5:** A plot obtained using Linear Discriminant Analysis (LDA) of the four
768 hyperspectral signature features A-D that varied significantly between morula
769 cultured in 7% and 20% O₂. The LDA helps to optimally separate the two classes
770 of embryos. Crosses = 7% O₂; circles = 20% O₂ treatment. Crosshairs = means of
771 the clusters. These means are significantly different (P < 0.001).

772

773 **Supplementary Material**

774 **Hyperspectral algorithms**

775 Our selection of the most informative cellular features arrived at the following
776 four best features (**Features 1-4**).

777

778 **Feature 1** refers to the log of the mean pixel intensity of the brightest 10% of
779 pixels in channel 5 (ex: 365 nm, em: 587 nm).

780

781 **Feature 2** calculations relate to the blobbiness of images (channel 8; ex: 495 nm,
782 em: 635 nm), a measure of the pixel intensity blobs values disorder. The blob
783 image intensity image was first filtered using a continuous wavelet transform
784 filter (Mexican hat wavelet). The multidimensional mexihat wavelet function is
785 equivalent to the laplacian of a multidimensional Gaussian:

786

$$787 \quad \square(\square, \square, \square) = -\frac{1}{\square\square^4} \left(1 - \frac{\square^2 + \square^2}{2\square^2} \right) \square^{-\frac{(\square^2 + \square^2)}{2\square^2}}$$

788

789 Where x and y are the matrix coordinates and σ is a scaling value. Small values
790 make the wavelet filter sensitive to fine spatial detail.

791

792 To calculate the wavelet filter output for a given input image, the image matrix of
793 intensity values was convoluted with the 2D wavelet function defined at a
794 particular scale value. The smallest scale starting at one provides a filter with the
795 highest frequency sensitivity producing high output values in regions where there
796 are very small blobs. This convolution was performed by transforming the wavelet
797 function matrix and image using the 2D fast Fourier transform algorithm,
798 multiplying the matrices element wise, then transforming the answer back into
799 the spatial domain (Antoine, et al., 2004). For the feature of interest in this work
800 (Feature 2), a scale value of 2 was used, and then the wavelets filtering were
801 performed. The wavelet-filtered images contained a high contrast pattern of many
802 small blobs.

803

804 Furthermore, the local entropy was determined, based on the calculation of pair-
805 wise entropy values of a centre pixel with its local neighbouring pixel intensities.
806 The size of the neighbourhood chosen here were nine pixels from the centre pixel.
807 Thus 360 neighbouring pixel intensity values were used to calculate entropy at
808 each pixel site. Each of the \square neighbour pixel intensity values were binned into
809 one of 16 intensity bins, equally spanning the 0-255 ranges of grey intensity levels.
810 From this, we construct an estimated probability distribution $\square(\square_\square)$ for the
811 neighbouring pixel intensity values occurring within a bin \square_\square .

812

813
$$\text{Local entropy} = - \sum_{\square} \square(\square_\square) \square \square \square_2 \square(\square_\square)$$

814

815 Maximum entropy or uncertainty occurs when distribution is normal or random,
816 therefore any local structure were likely to yield a lower entropy value. Local
817 entropy is defined for a specific pixel. To calculate the local entropy feature for a
818 cell, local entropies were added for each pixel in that cell.

819

820 **Feature 3** is the mean intensity ratio of channels 11 and 13. The mean pixel
821 intensity value of signal in channel 11 (ex: 425 nm, em: 587 nm) was divided by
822 the mean pixel intensity value of signal in channel 13 (ex: 455 nm, em: 587 nm).

823

824 **Feature 4** is the standard deviation of channel 15-pixel intensity. The pixel
825 intensity dispersion, as measured by the standard deviation, was calculated in
826 channel 15.

827