



## Long-term development of white matter fibre density and morphology up to 13 years after preterm birth: A fixel-based analysis

Claire E. Kelly<sup>a,b,\*</sup>, Deanne K. Thompson<sup>a,b,c,d</sup>, Sila Genc<sup>b,e</sup>, Jian Chen<sup>b</sup>, Joseph Y.M. Yang<sup>b,c,f,g</sup>, Chris Adamson<sup>b</sup>, Richard Beare<sup>b</sup>, Marc L. Seal<sup>b,c</sup>, Lex W. Doyle<sup>a,c,h,i</sup>, Jeanie L.Y. Cheong<sup>a,h,i</sup>, Peter J. Anderson<sup>a,j</sup>

<sup>a</sup> Victorian Infant Brain Study (VIBeS), Murdoch Children's Research Institute, Melbourne, Australia

<sup>b</sup> Developmental Imaging, Murdoch Children's Research Institute, Melbourne, Australia

<sup>c</sup> Department of Paediatrics, The University of Melbourne, Melbourne, Australia

<sup>d</sup> Florey Institute of Neuroscience and Mental Health, Melbourne, Australia

<sup>e</sup> Cardiff University Brain Research Imaging Centre (CUBRIC), Cardiff University, Cardiff, UK

<sup>f</sup> Department of Neurosurgery, The Royal Children's Hospital, Melbourne, Australia

<sup>g</sup> Neuroscience Research, Murdoch Children's Research Institute, Melbourne, Australia

<sup>h</sup> Newborn Research, The Royal Women's Hospital, Melbourne, Australia

<sup>i</sup> Department of Obstetrics and Gynaecology, The University of Melbourne, Melbourne, Australia

<sup>j</sup> Turner Institute for Brain and Mental Health, Monash University, Melbourne, Australia

### ARTICLE INFO

#### Keywords:

Prematurity  
Magnetic resonance imaging  
Diffusion imaging  
White matter  
Microstructure  
Longitudinal

### ABSTRACT

**Background:** It is well documented that infants born very preterm (VP) are at risk of brain injury and altered brain development in the neonatal period, however there is a lack of long-term, longitudinal studies on the effects of VP birth on white matter development over childhood. Most previous studies were based on voxel-averaged, non-fibre-specific diffusion magnetic resonance imaging (MRI) measures, such as fractional anisotropy. In contrast, the novel diffusion MRI analysis framework, fixel-based analysis (FBA), enables whole-brain analysis of microstructural and macrostructural properties of individual fibre populations at a sub-voxel level. We applied FBA to investigate the long-term implications of VP birth and associated perinatal risk factors on fibre development in childhood and adolescence.

**Methods:** Diffusion images were acquired for a cohort of VP (born <30 weeks' gestation) and full-term (FT, ≥37 weeks' gestation) children at two timepoints: mean (SD) 7.6 (0.2) years ( $n = 138$  VP and 32 FT children) and 13.3 (0.4) years ( $n = 130$  VP and 45 FT children). 103 VP and 21 FT children had images at both ages for longitudinal analysis. At every fixel (individual fibre population within an image voxel) across the white matter, we compared FBA metrics (fibre density (FD), cross-section (FC) and a combination of these properties (FDC)) between VP and FT groups cross-sectionally at each timepoint, and longitudinally between timepoints. We also examined associations between known perinatal risk factors and FBA metrics in the VP group.

**Results:** Compared with FT children, VP children had lower FD, FC and FDC throughout the white matter, particularly in the corpus callosum, tapetum, inferior fronto-occipital fasciculus, fornix and cingulum at ages 7 and 13 years, as well as the corticospinal tract and anterior limb of the internal capsule at age 13 years. VP children also had slower FDC development in the corpus callosum and corticospinal tract between ages 7 and 13 years compared with FT children. Within VP children, earlier gestational age at birth, lower birth weight z-score, and neonatal brain abnormalities were associated with lower FD, FC and FDC throughout the white matter at both ages.

**Conclusions:** VP birth and concomitant perinatal risk factors are associated with fibre tract-specific alterations to axonal development in childhood and adolescence.

\* Corresponding author. Murdoch Children's Research Institute, 50 Flemington Road, Parkville, Victoria, 3052, Australia.

E-mail address: [claire.kelly@mcri.edu.au](mailto:claire.kelly@mcri.edu.au) (C.E. Kelly).

<https://doi.org/10.1016/j.neuroimage.2020.117068>

Received 28 February 2020; Received in revised form 3 May 2020; Accepted 15 June 2020

Available online 22 June 2020

1053-8119/© 2020 The Author(s). Published by Elsevier Inc. This is an open access article under the CC BY-NC-ND license (<http://creativecommons.org/licenses/by-nc-nd/4.0/>).

## 1. Introduction

Preterm birth is a significant clinical and public health concern given the large and increasing number of infants who survive with serious health and developmental problems (approximately 11% of births are preterm at <37 weeks' gestation and approximately 1.8% are very preterm (VP) at <32 weeks' gestation) (Saigal and Doyle, 2008; Blencowe et al., 2012). Preterm infants are susceptible to brain injury, particularly white matter injury, and subsequent disruptions to the normal development of both the white matter and grey matter (Volpe, 2019). The manifestations of brain injury and altered brain maturation can be assessed using magnetic resonance imaging (MRI), with diffusion-weighted MRI providing an unprecedented method for studying white matter on the microscopic scale. White matter microstructural disturbances in VP infants have clinical relevance due to their association with a range of motor, cognitive and behavioural delays (Barnett et al., 2018).

A major challenge in analysing diffusion images is accounting for the complex, crossing fibre geometries in the white matter, which are present in up to 90% of white matter image voxels (Jeurissen et al., 2013). The most common diffusion image analysis approach, diffusion tensor imaging (DTI), cannot resolve crossing fibres, meaning the microstructural parameters derived from DTI (fractional anisotropy and axial, radial and mean diffusivities) are not fibre-specific, which leads to complicated and potentially even erroneous interpretations of DTI findings in regions containing crossing fibres (Jones et al., 2013). In contrast, the recently developed fixel-based analysis (FBA) framework is based on a model of multiple fibre orientations within voxels (constrained spherical deconvolution) (Tournier et al., 2007). Because of this, FBA is able to characterise microstructural properties of each 'fixel' (specific fibre population in any direction within an image voxel) (Raffelt et al., 2017). In addition, FBA characterises morphological (macrostructural) properties of specific fibre populations. The FBA framework enables statistical analysis of the following parameters at every fixel across the whole-brain white matter: fibre density (FD), a microstructural measure of changes in the density of axons within a fibre population; fibre cross-section (FC), a macrostructural measure of changes in the cross-sectional area that a fibre population occupies, and; fibre density and cross-section (FDC), a combined measure of both of these microstructural and macrostructural properties (Raffelt et al., 2017). Decreases in FD can indicate axonal loss, whereas decreases in FC can indicate macroscopic fibre atrophy in diseases such as Alzheimer's disease and multiple sclerosis (Gajamange et al., 2018; Mito et al., 2018; Rojas-Vite et al., 2019).

Previous studies have clearly documented the impact of preterm birth and associated perinatal risk factors on FBA metrics during the neonatal period (Pannek et al., 2018; Pecheva et al., 2019). Infants born <31 weeks' gestation and scanned at 38–44 weeks' postmenstrual age had lower FD, FC and FDC in the corpus callosum, fornix, anterior commissure, optic radiation, cerebral and cerebellar peduncles, cingulum and superior longitudinal fasciculus compared with full-term (FT, born 38–41 weeks' gestation) infants (Pannek et al., 2018). In the same study, brain abnormality scored using the neonatal MRI scoring system of Kidokoro et al. (2013) was associated with reduced FD in the corpus callosum (Pannek et al., 2018). In another study, earlier gestational age at birth and lower birth weight were associated with lower FD, FC and FDC in a number of white matter fibre tracts in infants born <33 weeks' gestation and scanned at 38–47 weeks' postmenstrual age (Pecheva et al., 2019).

However, there have been no published applications of FBA to preterm populations beyond the neonatal period. Furthermore, there have been few longitudinal studies of white matter development during childhood and adolescence following preterm birth compared with FT birth; none using FBA and very few using DTI (Jo et al., 2012; Thompson et al., 2015). As such, there is a need for long-term, longitudinal studies using advanced analysis methods to expand knowledge on the effects of VP birth on white matter development. In the current study, we apply the recently developed FBA framework to investigate the long-term

implications of VP birth and associated perinatal risk factors on fibre microstructure and macrostructure over childhood and adolescence.

## 2. Methods

### 2.1. Participants

A total of 224 infants born VP (specifically, <30 weeks' gestation or <1250 g) without genetic or congenital abnormalities were recruited between July 2001 and December 2003 from the Royal Women's Hospital, Melbourne, into a prospective longitudinal cohort study. A total of 76 infants born FT ( $\geq 37$  weeks' gestation) were also recruited; 45 at birth and 31 at 2 years of age. The participants were invited to return for MRI at ages 7 and 13 years; 159 VP and 35 FT children had MRI at 7 years of age, and 141 VP and 47 FT children had MRI at 13 years of age. Following exclusions during image processing due to incomplete or incorrect image acquisitions or movement artefact, there were 138 VP and 32 FT children who were included in the cross-sectional analysis at 7 years of age, and 130 VP and 45 FT children who were included in the cross-sectional analysis at 13 years of age. Of these, 103 VP and 21 FT children had images at both ages for longitudinal analysis. The study was approved by the Human Research and Ethics Committees of the Royal Women's Hospital and the Royal Children's Hospital, Melbourne. Parents gave written informed consent for their child to participate.

### 2.2. Perinatal data

Perinatal data included gestational age at birth, sex, and birth weight standardised for gestational age and sex (birth weight z-score) (Cole et al., 1998). Major neonatal brain injuries (intraventricular haemorrhage (Papile et al., 1978) and cystic periventricular leukomalacia) were diagnosed from serial cranial ultrasounds prior to term in the VP group. Additionally, the presence and severity of brain abnormalities were assessed from MRI at term-equivalent age using a semi-qualitative scoring system (Kidokoro et al., 2013). A global brain abnormality score was calculated by summing abnormality scores across the white matter, cortical and deep grey matter, and cerebellum. Higher global brain abnormality scores indicate more severe brain abnormalities.

### 2.3. MRI acquisition

At both the 7-year and 13-year follow-ups, MRI was conducted using a 3T scanner (Siemens Tim Trio, Erlangen, Germany).

At the 7-year follow-up, images acquired included  $T_1$ -weighted images (3D ultrafast magnetization-prepared rapid gradient-echo (MP-RAGE) sequence, flip angle =  $9^\circ$ , repetition time = 1900 ms, echo time = 2.27 ms, field of view =  $210 \times 210$  mm, matrix size =  $256 \times 256$ , echo spacing = 6.9 ms, voxel size = 0.8 mm isotropic, and acquisition time = 4 min 33 s) and diffusion-weighted images (twice-refocused echo planar imaging sequence, 45 gradient directions at  $b$ -value =  $3000 \text{ s/mm}^2$ , six  $b = 0 \text{ s/mm}^2$  volumes, repetition time = 7400 ms, echo time = 106 ms, field of view =  $240 \times 240$  mm, matrix size =  $104 \times 104$ , voxel size = 2.3 mm isotropic, and acquisition time = 6 min 52 s).

At the 13-year follow-up, images acquired included  $T_1$ -weighted images (3D multi-echo MP-RAGE sequence with prospective motion correction, repetition time 2530 = ms, echo times = 1.77, 3.51, 5.32 and 7.2 ms, flip angle =  $7^\circ$ , field of view =  $230 \times 209$  mm, matrix =  $256 \times 230$ , interpolated =  $256 \times 256$ , voxel size = 0.9 mm isotropic, and acquisition time = 6 min 52 s) and diffusion-weighted images (multi-band accelerated echo planar imaging pulse sequence, 60 gradient directions at  $b$ -value =  $2800 \text{ s/mm}^2$ , four  $b = 0 \text{ s/mm}^2$  images, repetition time = 3200 ms, echo time = 110 ms, field of view =  $260 \times 260$  mm, matrix size =  $110 \times 110$ , voxel size = 2.4 mm isotropic, multi-band acceleration factor = 3, and acquisition time = 3 min 57 s). A pair of  $b = 0 \text{ s/mm}^2$  images with reversed phase encoding (anterior-posterior and posterior-anterior) were also acquired.

## 2.4. Diffusion image pre-processing

Diffusion images were brain extracted using the Brain Extraction Tool (BET) from the functional MRI of the Brain (FMRIB) Software Library (FSL; version 5.0.11) (Smith, 2002). Brain masks were manually checked and edited as required. 7-year images were corrected for: (1) movement and eddy current-induced distortions [using the FSL ‘eddy’ tool with slice-to-volume motion correction, outlier detection and replacement, and *b*-vector reorientation (Andersson and Sotiropoulos, 2016; Andersson et al., 2016, 2017; Leemans and Jones, 2009)] and; (2) susceptibility-induced distortions [based on information from the  $T_1$ -weighted images using BrainSuite version 18 (Bhushan et al., 2012)]. 13-year images were corrected for: (1) susceptibility-induced distortions [based on information from the reversed phase-encoded images using the FSL ‘topup’ tool (Andersson et al., 2003)] and; (2) motion and eddy-current-induced distortions [the FSL ‘eddy’ tool with slice-to-volume motion correction, outlier detection and replacement, and *b*-vector reorientation (Andersson and Sotiropoulos, 2016; Andersson et al., 2016, 2017; Leemans and Jones, 2009)]. We visually examined corrected diffusion images, and also obtained quantitative metrics relating to image quality using the FSL QUality Assessment for DMRI (QUAD) and Study-wise QUality Assessment for DMRI (SQUAD) tools (Bastiani et al., 2019); this information resulted in exclusion of four images from the 7-year follow-up and one image from the 13-year follow-up. For the remaining images that were suitable for inclusion, quality control metrics generally did not differ between the VP and FT groups, but many metrics were poorer for the 7-year images compared with the 13-year images (Supplementary Table 1).

## 2.5. Fixel-based analysis

Following pre-processing, images were analysed using recommended steps for a single-shell, single-tissue FBA (Raffelt et al., 2017) in MRtrix3 (version 3.0\_RC3) (Tourneris et al., 2019). Images were corrected for bias fields (Tustison et al., 2010). Global intensity normalisation was performed based on all images. Images were then upsampled to  $1.3 \text{ mm}^3$ . Constrained spherical deconvolution was performed on all images using an average response function made from all images (Tourneris et al., 2013), resulting in fibre orientation distributions (FOD).

30 participants (15 VP and 15 FT) were randomly selected from each follow-up to generate a 7-year and a 13-year study-specific FOD template for the cross-sectional analyses. The total 60 images were used to generate a template for longitudinal analyses. Each of the three templates (7-year, 13-year and longitudinal) were separately created by iteratively normalising and averaging the selected participants’ FOD images using a symmetric diffeomorphic FOD registration algorithm (Raffelt et al., 2011), implemented via the ‘population\_template’ script within MRtrix3. Participants with major neonatal brain injuries were excluded from the template subset, consistent with previous studies (Pecheva et al., 2019). Age and sex ratio in the template subset did not differ to that of the remaining participants (all  $p > 0.1$ ).

7-year and 13-year FOD images were registered to their respective FOD template, and all FOD images were registered to the longitudinal FOD template. We visually examined registrations, and excluded one 7-year VP image that had poor registration as a result of brain abnormalities. In all three template spaces, fixels were segmented and FBA metrics (FD, FC in log form, and FDC) were calculated as previously described (Raffelt et al., 2017). Whole brain tractography was performed on the FOD templates, with spherical-deconvolution informed filtering of tractograms (SIFT) (Smith et al., 2013), which is required for statistical analysis using the connectivity-based fixel enhancement (CFE) method (Raffelt et al., 2015).

## 2.6. Statistical analysis

In the current study we performed whole-brain fixel-based analyses

only, i.e. all statistical analyses were performed at the level of each fixel across the whole-brain white matter.

At each fixel, we compared FD, FC and FDC between the VP and FT groups separately at ages 7 and 13 years using a General Linear Model. These cross-sectional analyses were performed in the space of the respective cross-sectional template. All comparisons were adjusted for age and sex, and comparisons of FC and FDC were repeated adjusting for intracranial volume (generated from the  $T_1$ -weighted images using Statistical Parametric Mapping version 12), consistent with previous studies (Raffelt et al., 2017; Pannek et al., 2018; Pecheva et al., 2019). Connectivity-based smoothing and statistical inference were performed using CFE (Raffelt et al., 2015). Non-parametric permutation testing (5000 permutations) was used to generate a family-wise error rate (FWE)-corrected  $p$ -value for every individual fixel.

Again, using a General Linear Model, CFE and non-parametric permutation testing, we compared longitudinal changes in FD, FC and FDC at each fixel from age 7–13 years between the VP and FT groups, adjusting for change in age, sex and change in intracranial volume. To enable these longitudinal analyses, we subtracted each participant’s 7-year FD, FC and FDC image from their 13-year FD, FC and FDC image, and statistical comparisons were performed on the difference in FD, FC and FDC between ages. Furthermore, a modified version of CFE was used to enable the longitudinal analyses, as previously detailed (Genc et al., 2018). These longitudinal analyses were performed in the space of the longitudinal template.

As a secondary analysis, we repeated the above cross-sectional and longitudinal comparisons of FBA metrics at each fixel between the VP and FT groups excluding the subset of VP children who had intraventricular haemorrhage grade 3 or 4 and/or cystic periventricular leukomalacia, to ensure any group differences in FBA metrics were not driven by this subset.

Finally, using the same methods described above, in the VP group, we examined associations between perinatal data (gestational age at birth, birth weight z-score, sex, and neonatal global brain abnormality score) and: (1) FD, FC and FDC at each fixel at ages 7 and 13 years, and; (2) longitudinal changes in FD, FC and FDC at each fixel between ages 7 and 13 years. Again, cross-sectional analyses were performed in the space of the cross-sectional templates and longitudinal analyses in the space of the longitudinal templates.

Fixels were considered statistically significant at  $p < 0.05$ , FWE-corrected. Significant fixels were anatomically localised by visual inspection with reference to the JHU white matter atlas (Oishi et al., 2011). The results section focuses on major results that were confirmed in secondary analyses.

## 2.7. Data availability statement

The data analysed during the current study are available from the corresponding author on reasonable request and completion of a data sharing agreement. The data are not publicly available due to ethical restrictions.

## 3. Results

### 3.1. Participant characteristics

The proportion of males and females did not differ significantly between the VP and FT groups (Table 1). The rate of major neonatal brain injuries was relatively low in the VP group. Neonatal global brain abnormality score was higher in the VP group compared with the FT group. Age at each MRI was similar for the VP and FT groups. Intracranial volume was smaller in the VP group than the FT group at ages 7 and 13 years.

Characteristics of the included participants were generally similar to those of the non-participants (the participants, of the original  $n = 224$  VP and  $n = 76$  FT participants, who were recruited into the study but could

**Table 1**

Characteristics of the participants included in the fixel-based analysis, separated by age (7 years and 13 years) and group (very preterm (VP) and full-term (FT)).

Characteristic	Age 7 years			Age 13 years		
	VP, n = 138	FT, n = 32	p-value (VP-FT)	VP, n = 130	FT, n = 45	p-value (VP-FT)
Gestational age at birth (weeks), mean (SD)	27.5 (1.9)	38.9 (1.3)	NA	27.4 (1.9)	39.0 (1.4)	NA
Birth weight (grams), mean (SD)	977 (224)	3247 (509)	NA	964 (230)	3316 (552)	NA
Females, n (%)	71 (51)	17 (53)	0.86	61 (47)	23 (51)	0.63
Intraventricular haemorrhage grade 3 or 4, n (%)	5 (4)	NA	NA	7 (5)	NA	NA
Cystic periventricular leukomalacia, n (%)	4 (3)	NA	NA	4 (3)	NA	NA
Neonatal global brain abnormality score, mean (SD)	5.07 (2.89) <sup>a</sup>	1.72 (1.44)	<0.001	5.25 (3.00)	1.50 (1.41) <sup>d</sup>	<0.001
Age at MRI (years), mean (SD)	7.5 (0.2)	7.6 (0.2)	0.17	13.3 (0.4)	13.3 (0.5)	0.97
Intracranial volume (cm <sup>3</sup> ), mean (SD)	1339 (114) <sup>b</sup>	1432 (102) <sup>c</sup>	<0.001	1441 (132)	1526 (157)	<0.001

<sup>a</sup> n = 137.

<sup>b</sup> n = 135.

<sup>c</sup> n = 30 (there were 5 participants at the 7-year follow-up who were included in the fixel-based analysis but were missing intracranial volume data, because their T<sub>1</sub>-weighted images had movement artefact and/or tissue segmentation failed for these participants, despite them having good quality diffusion-weighted images).

<sup>d</sup> n = 24.

not be followed up or were excluded from the current analysis). However, included VP participants had lower neonatal global brain abnormality scores than VP non-participants (for the 7-year follow-up sample, mean (SD) = 5 (3) versus 7 (4),  $p = 0.001$ ; for the 13-year follow-up sample, mean (SD) = 5 (3) versus 6 (4),  $p = 0.03$ ).

### 3.2. Group differences

VP children had significantly lower FD, FC and FDC than FT children in many fixels located throughout many major fibre tracts at ages 7 and 13 years (all  $p_{FWE} < 0.05$ ; Fig. 1A;  $p$ -values for each significant fixel are shown in Supplementary Fig. 1A; locations of significant fixels are listed in Supplementary Table 2). At age 7 years, FD was 21% lower on average across all significant fixels in VP children compared with FT children (Fig. 1B). FC group differences were smaller in magnitude, but more widespread across the white matter, than the FD differences. A similar pattern was observed at age 13 years; FD was on average 16% lower in the VP group compared with the FT group, and again FC differences were smaller in magnitude but more widespread than the FD differences. Additionally, more fixels differed between groups at age 13 years than 7 years; for example, 7% of fixels (35146 significant fixels out of 527417 fixels in the 7-year white matter template analysis fixel mask) versus 13% of fixels (78832 significant fixels out of 585732 fixels in the 13-year white matter template analysis fixel mask) at ages 7 and 13 years respectively had lower FC in the VP group compared with the FT group. The FC and FDC group differences at both ages were no longer significant after adjusting for intracranial volume (all  $p_{FWE} \geq 0.05$ ). There were no fixels in which VP children had higher FD, FC or FDC than FT children at

age 7 or 13 years, except for a very small number of fixels (0.01% of all fixels analysed) in the superior longitudinal fasciculus with significantly higher FD in the VP group than the FT group at age 13 years (all  $p_{FWE} < 0.05$ ; Supplementary Table 2).

Between ages 7 and 13 years, FDC in fixels located in the splenium of the corpus callosum, right cerebral peduncle and right posterior limb of the internal capsule increased significantly less in VP children compared with FT children, even after adjusting for intracranial volume (all  $p_{FWE} < 0.05$ ; Fig. 2A; Supplementary Fig. 1B). In these fixels, the increase over time was on average 26% lower in the VP group compared with the FT group (Fig. 2B).

The cross-sectional and longitudinal group differences in FBA metrics remained significant after excluding the VP children who had intraventricular haemorrhage grade 3 or 4 and/or cystic periventricular leukomalacia (all  $p_{FWE} < 0.05$ ; Supplementary Fig. 2).

### 3.3. Perinatal factors

Earlier gestational age at birth was significantly associated with lower FD, FC and FDC in fixels located in several fibre tracts, particularly the corpus callosum, tapetum and anterior commissure, at ages 7 and 13 years (all  $p_{FWE} < 0.05$ ; Fig. 3; Supplementary Fig. 3). Lower birth weight z-score was significantly associated with lower FC and FDC in many fixels located throughout the white matter at both ages (all  $p_{FWE} < 0.05$ ; Fig. 4; Supplementary Fig. 4). For both gestational age at birth and birth weight z-score, associations with FC and FDC were not significant after adjusting for intracranial volume (all  $p_{FWE} \geq 0.05$ ). There were no associations in the opposite direction, except for in a small number of fixels ( $\leq 0.1\%$  of all the fixels analysed), where earlier gestational age and lower birth weight z-score were associated with higher FD in the left superior longitudinal fasciculus, and splenium and bilateral fornix respectively, at age 13 years (all  $p_{FWE} < 0.05$ ).

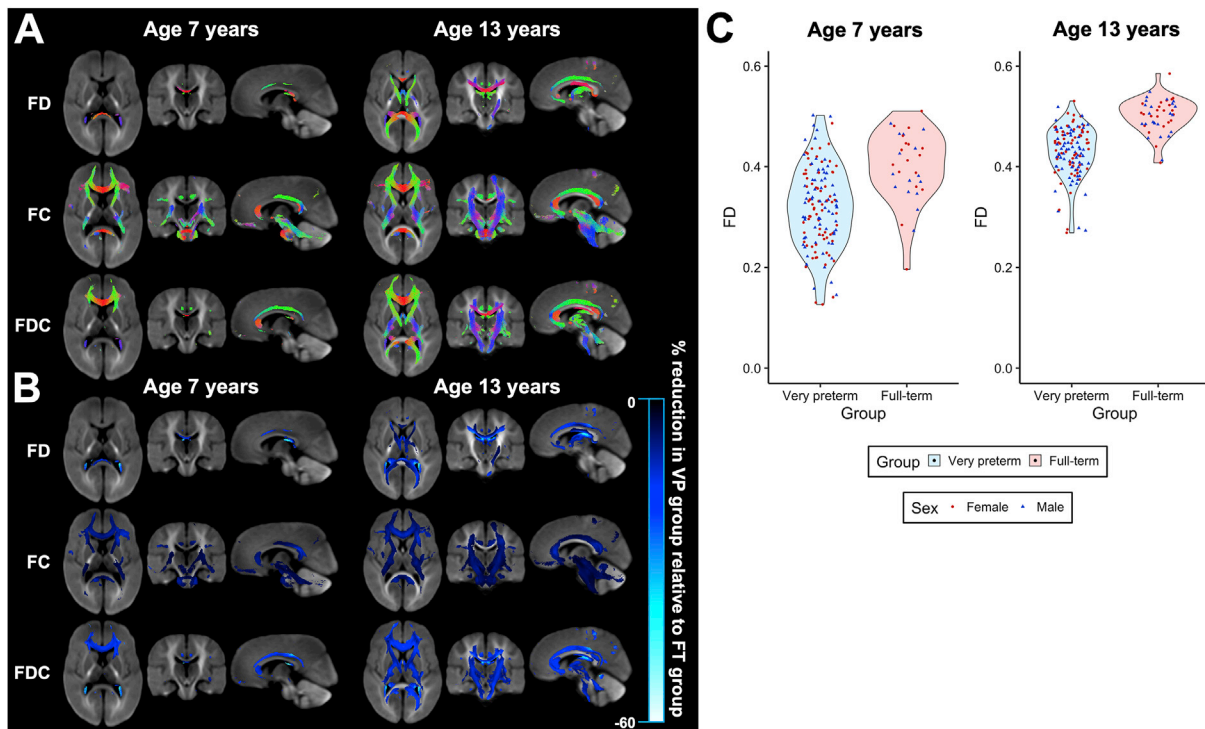
VP males had significantly larger FC and FDC in fixels located throughout the white matter compared with VP females at ages 7 and 13 years (all  $p_{FWE} < 0.05$ ), although these differences were no longer significant after adjusting for intracranial volume (all  $p_{FWE} \geq 0.05$ ). Between ages 7 and 13 years, VP females had a significantly greater increase in FC in fixels located in the corpus callosum than VP males, even after adjusting for intracranial volume (all  $p_{FWE} < 0.05$ ; Fig. 5; Supplementary Fig. 5). However, post-hoc analyses revealed that these sex-based differences in FBA metrics did not vary significantly between the VP and FT groups (all sex-by-group interaction  $p_{FWE} \geq 0.05$ ).

Higher neonatal global brain abnormality scores were significantly associated with lower FD, FC and FDC in many fixels located throughout the white matter at ages 7 and 13 years (all  $p_{FWE} < 0.05$ ), although the associations with FC and FDC were no longer significant after adjusting for intracranial volume (all  $p_{FWE} \geq 0.05$ ). Higher neonatal global brain abnormality scores were also significantly associated with less increase in FDC in fixels located in the corpus callosum between ages 7 and 13 years, even after adjusting for intracranial volume (all  $p_{FWE} < 0.05$ ; Fig. 6; Supplementary Fig. 6).

## 4. Discussion

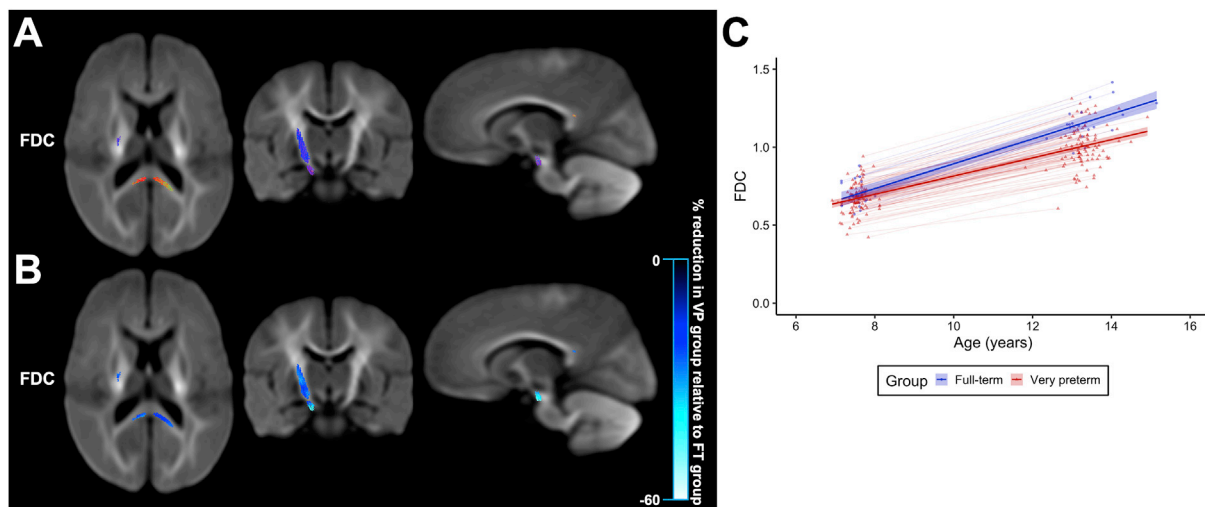
We have presented a unique long-term, longitudinal study of white matter development up to 13 years after VP birth in comparison with FT birth. Using the recently developed FBA framework, we revealed several fibre tract-specific findings: (1) VP children have axonal reductions across many fibre tracts at ages 7 and 13 years compared with FT children; (2) VP children have slower axonal growth over time specifically in the corpus callosum and corticospinal tract, and; (3) earlier gestational age at birth, lower birth weight, and neonatal brain abnormalities are important perinatal factors associated with later axonal alterations within the VP population.

At high diffusion weightings ( $b$ -values  $\geq 3000$  s/mm<sup>2</sup>), the extra-axonal water signal is strongly attenuated, leaving the remaining signal



**Fig. 1.** Cross-sectional group differences in fixel-based analysis metrics.

The figures were generated by cropping the whole-brain template-derived tractogram so that it included only streamline segments that pass through fixels that had significantly lower fibre density (FD), fibre cross-section (FC), and fibre tractography and cross-section (FDC) in the very preterm (VP) group compared with the full-term (FT) group cross-sectionally at ages 7 and 13 years ( $p < 0.05$ , family-wise error rate-corrected). Streamline segments were then coloured by (A) direction (anterior-posterior = green; superior-inferior = blue; left-right = red) and (B) the percentage reduction in FD, FC or FDC in the VP group compared with the FT group. In (C), FD values at age 7 (left) and 13 (right) years, averaged across the significant fixels in (A) and (B), are shown as violin plots. All significant results presented were obtained from models adjusted for age and sex. For FC and FDC, there were no significant fixels after additionally adjusting for intracranial volume.

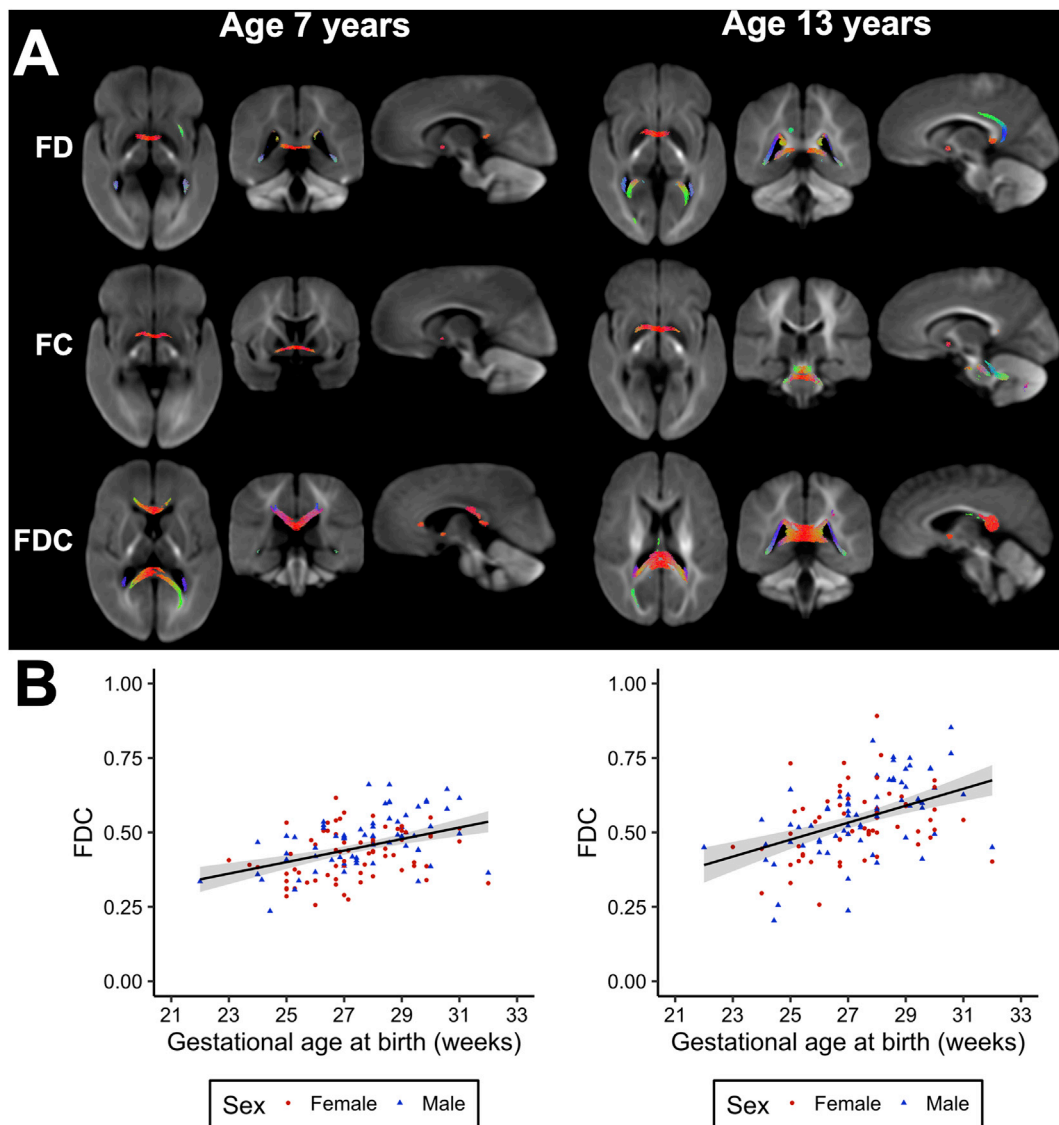


**Fig. 2.** Longitudinal group differences in fixel-based analysis metrics.

The figures were generated by cropping the whole-brain template-derived tractogram so that it included only streamline segments that pass through fixels in which fibre density and cross-section (FDC) increased significantly less between ages 7 and 13 years in the very preterm (VP) group compared with the full-term (FT) group ( $p < 0.05$ , family-wise error rate-corrected). Streamline segments were then coloured by (A) direction (anterior-posterior = green; superior-inferior = blue; left-right = red) and (B) the percentage by which the VP group increased less over time compared with the FT group. In (C), FDC values averaged across the significant fixels in (A) and (B) have been plotted against age. All significant results presented were obtained from models adjusted for change in age, sex and change in intracranial volume.

localised to the intra-axonal water compartment, and allowing us to make fibre-specific inferences using FBA (Raffelt et al., 2017; Genc et al., 2020). The observed lower FD in VP children compared with FT children suggests VP children have lower axonal densities within fibre tracts,

which could reflect axon loss or smaller axonal diameters (Raffelt et al., 2012). In addition to microstructural differences within fibre tracts, the lower FC in VP children compared with FT children suggests VP children also have lower total cross-sectional area of fibre tracts. Additionally,



**Fig. 3.** Associations between gestational age at birth and fixel-based analysis metrics.

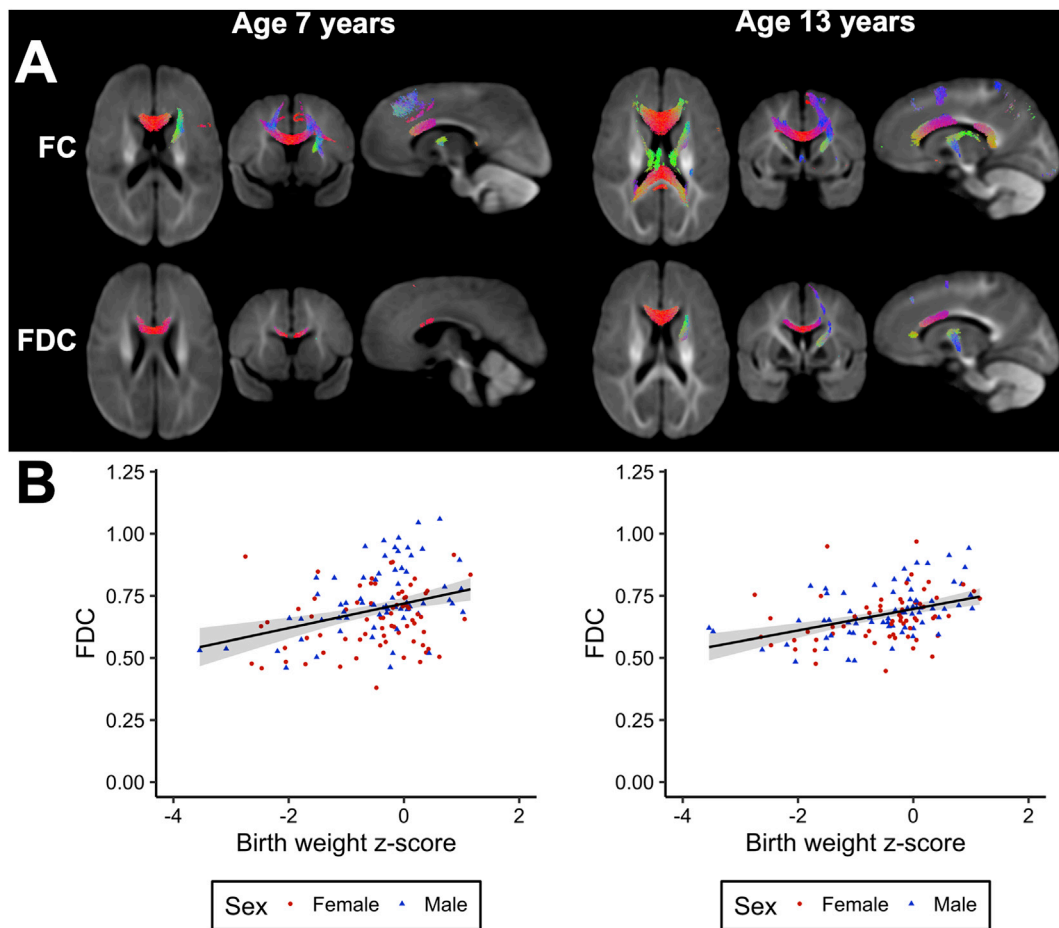
In part A, the figures were generated by cropping the whole-brain template-derived tractogram so that it included only streamline segments that pass through fixels in which earlier gestational age at birth was significantly associated with lower fibre density (FD), fibre cross-section (FC) and fibre density and cross-section (FDC) cross-sectionally at ages 7 and 13 years in the very preterm (VP) group ( $p < 0.05$ , family-wise error rate-corrected). Streamline segments were then coloured by direction (anterior-posterior = green; superior-inferior = blue; left-right = red). In part B, FDC values at age 7 (left) and 13 (right) years, averaged across the significant fixels in part A, have been plotted against gestational age at birth. All significant results presented were obtained from models adjusted for age and sex. For FC and FDC, there were no significant fixels after additionally adjusting for intracranial volume.

lower myelin content could increase the exchange of water between the intra-axonal and extra-axonal spaces, resulting in an apparent decrease in the volume of the intra-axonal compartment, and hence a decrease in FD (Pannek et al., 2018; Raffelt et al., 2012). Therefore, the current results could also suggest that VP children have lower myelin content than FT children. These findings suggest there is a decreased capacity to transfer information between brain regions in VP children compared with FT children (Raffelt et al., 2017).

VP children had lower FD in many specific fibre pathways compared with FT children. The fibre tracts predominantly affected included the corpus callosum, tapetum, inferior fronto-occipital fasciculus, fornix and cingulum at both ages, as well as the corticospinal tract and anterior limb of the internal capsule at age 13 years. These fibre tracts are rapidly developing during childhood (Lebel and Beaulieu, 2011), suggesting VP children have axonal reductions in developmentally sensitive regions. The group differences in FC and FDC were located in similar but more widespread tracts. However, they were no longer significant after

adjusting for intracranial volume, indicating that macrostructural axonal reductions in VP children compared with FT children are commensurate with the known smaller head size in VP children (Monson et al., 2016). Our findings are consistent with previous studies at term-equivalent age (Pannek et al., 2018), suggesting that early axonal reductions are still present in childhood and adolescence. Our findings are also broadly in line with many previous studies based on non-fibre-specific diffusion MRI measures such as DTI and Neurite Orientation Dispersion and Density Imaging (NODDI) measures, which also report altered microstructure (commonly lower fractional anisotropy and higher diffusivities) across much of the white matter in preterm-born children and young adults compared with term-born controls (Skranes et al., 2007; Vangberg et al., 2006; Constable et al., 2008; Hollund et al., 2018; Eikenes et al., 2011; Allin et al., 2011; Young et al., 2019; Pascoe et al., 2019; Li et al., 2015; Pandit et al., 2013), including in the same cohort as the current study (Kelly et al., 2016).

In the premature brain an initial insult such as hypoxia, ischemia or



**Fig. 4.** Associations between birth weight z-score and fixel-based analysis metrics.

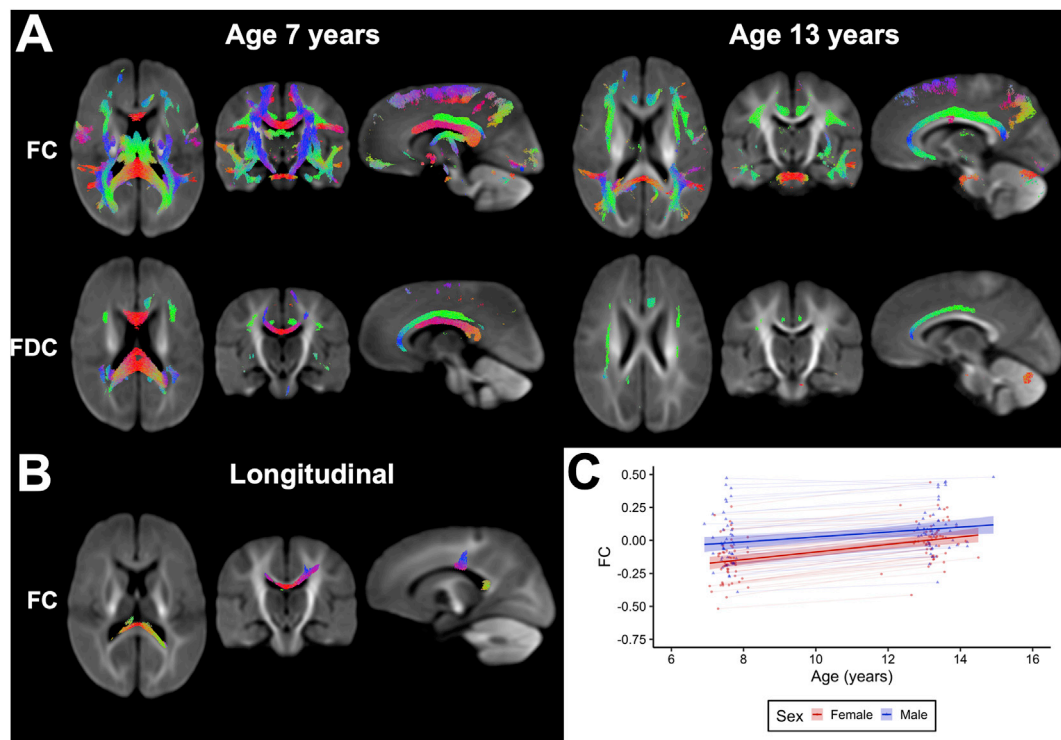
In part A, the figures were generated by cropping the whole-brain template-derived tractogram so that it included only streamline segments that pass through fixels in which lower birth weight z-score was significantly associated with lower fibre cross-section (FC) and fibre density and cross-section (FDC) cross-sectionally at ages 7 and 13 years in the very preterm (VP) group ( $p < 0.05$ , family-wise error rate-corrected). Streamline segments were then coloured by direction (anterior-posterior = green; superior-inferior = blue; left-right = red). In part B, FDC values at age 7 (left) and 13 (right) years, averaged across the significant fixels in part A, have been plotted against birth weight z-score. All significant results presented were obtained from models adjusted for age and sex. For FC and FDC, there were no significant fixels after additionally adjusting for intracranial volume.

inflammation is thought to lead to injury of pre-myelinating oligodendrocytes, followed by impaired myelination and axonal growth (Volpe, 2019). Recently, lower FC measured using FBA in the periventricular white matter, hippocampus and cerebellar white matter was related to histological markers of hypomyelination and axonal disorganisation in a growth-restricted, preterm animal model (Malhotra et al., 2019). The lower FC and histological abnormalities were found immediately after preterm birth, indicating the white matter injury occurred antenatally (Malhotra et al., 2019). Our study provides *in vivo* markers of the long-term effects of possible underlying antenatal white matter injury and/or altered development in VP children.

Longitudinally, VP children had slower FDC development in the splenium of the corpus callosum and right corticospinal tract between ages 7 and 13 years than FT children. Previous diffusion MRI studies have shown that typical white matter development is most rapid in the fetal and early postnatal period, but there is ongoing white matter development over childhood and adolescence in the form of increasing axonal density and myelination (Genc et al., 2017a, 2018; Lebel and Beaulieu, 2011; Geeraert et al., 2019; Dubois et al., 2014). In the corpus callosum (whose development was affected in our VP sample) the number of axons is typically close to a maximum at birth after which no new axons are formed, but structural changes including axonal pruning, redirection and myelination occur, which are more pronounced in the posterior (splenium) than anterior (genu) subdivisions (Dubois et al., 2014; Luders

et al., 2010). Therefore, our results may reflect reduced axonal growth (less increase in axonal diameter) and/or reduced myelination specifically in the splenium and right corticospinal tract between ages 7 and 13 years in VP children compared with FT children. Interestingly, significant group differences in corticospinal tract development were found in the right hemisphere only. Based on the statistical analysis performed, it is not possible to determine whether this was related to cerebral asymmetry (Dubois et al., 2009; Kwon et al., 2015) or simply a lack of power to detect significant results in the other hemisphere. Future studies may be worthwhile to investigate this further.

Earlier gestational age at birth, lower birth weight z-score and neonatal brain abnormalities were related to lower FD, FC and/or FDC in many specific fibre pathways at both ages; neonatal brain abnormalities were additionally related to slower change in FDC in the corpus callosum over time. This agrees with previous findings at term-equivalent age (Pannek et al., 2018; Pecheva et al., 2019). We also found VP males had larger FC and FDC throughout the white matter than VP females, proportional to their larger intracranial volume. Equivalent sex-based differences in FBA metrics were found previously in the neonatal period (Pecheva et al., 2019). In our study, we additionally found that VP females had faster axonal growth in the corpus callosum than VP males. This could reflect the developmental vulnerability of VP males that has been previously documented (Wood et al., 2005), however given that we found that sex-based differences in FBA metrics were similar between the



**Fig. 5.** Differences in fixel-based analysis metrics between very preterm (VP) males and VP females.

The figures were generated by cropping the whole-brain template-derived tractogram so that it included only streamline segments that pass through fixels in which (A) fibre cross-section (FC) and fibre density and cross-section (FDC) were significantly higher in VP males compared with VP females at ages 7 and 13 years, and (B) FC increased significantly more over time in VP females compared with VP males ( $p < 0.05$ , family-wise error rate-corrected). Streamline segments were then coloured by direction (anterior-posterior = green; superior-inferior = blue; left-right = red). In (C), FC values averaged across the significant fixels in (B) have been plotted against age, separately for VP males and VP females. In part A, all significant results presented were obtained from models adjusted for age; for FC and FDC, there were no significant fixels after additionally adjusting for intracranial volume. In part B, all significant results presented were obtained from models adjusted for change in age and change in intracranial volume.

VP and FT groups, our findings may be more likely to reflect typical sex-based developmental differences or influences of puberty (Genc et al., 2017b, 2018).

This study is strengthened by the large cohort of VP children and FT controls followed up over a long period of time. Some participants could not be followed up, however included participants were generally representative of the originally recruited sample, except they had lower neonatal brain abnormality scores. This suggests results may have been even more pronounced had all of the recruited participants been included. We acknowledge there were differences in MRI sequences (including lack of reverse phase-encoded images at the 7-year timepoint, which precluded susceptibility-induced distortion correction using the FSL ‘topup’ tool) and image quality between the 7-year and 13-year follow-ups, which could influence the longitudinal analysis. However, the image sequences, processing and quality were consistent between the VP and FT groups, which was the primary comparison in the current study. Future studies using identical image sequences between time-points would be valuable to validate our results. Additionally, we performed a whole-brain FBA, however future work to also segment individual fibre tracts and analyse each tract separately would be beneficial for specifying effect sizes and  $p$ -values for specific tracts. This would also enable more comprehensive mixed modelling of longitudinal data with repeated measurements (Genc et al., 2019). Furthermore, we performed linear modelling, but white matter development may be better described by non-linear models (Lebel and Beaulieu, 2011), and thus future studies investigating possible non-linear patterns of development in FBA metrics would be worthwhile. Lastly, our results in some regions should be interpreted with caution. Any registration inaccuracies and partial volume effects are most pronounced in thin structures and structures proximal to the ventricles (Djamanakova et al., 2013), making

it difficult to interpret results in these regions; for example, it can be difficult to distinguish differences in FD and FC in the fornix and anterior commissure (Raffelt et al., 2017; Pannek et al., 2018).

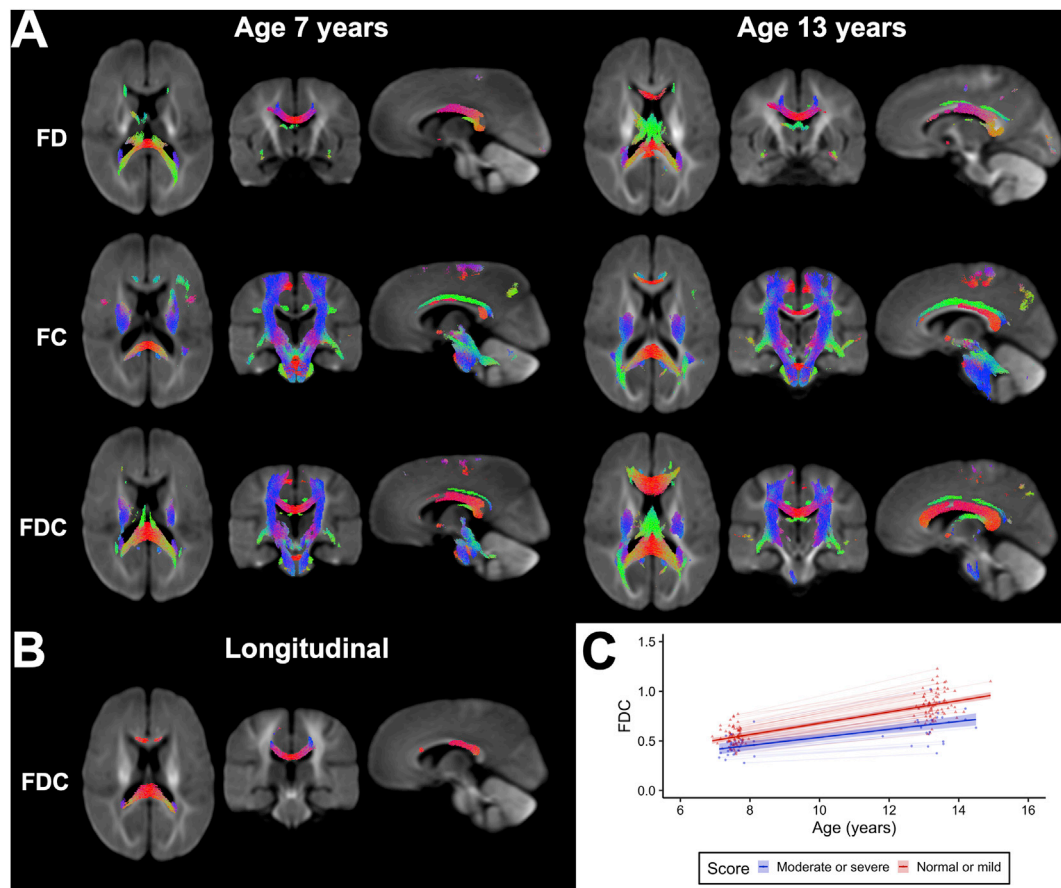
## 5. Conclusions

Using a long-term, longitudinal study design combined with advanced diffusion MRI, we found that VP birth and concomitant perinatal risk factors are associated with fibre-specific disruptions to axonal development, up to 13 years after birth. Understanding the specific white matter fibre properties such as density and cross-section affected by VP birth may in future enable identification of at-risk children and development of targeted interventions to improve outcomes for the vulnerable VP population.

## CRediT authorship contribution statement

**Claire E. Kelly:** Formal analysis, Investigation, Visualization, Writing - original draft, Writing - review & editing. **Deanne K. Thompson:** Conceptualization, Resources, Writing - review & editing, Supervision, Funding acquisition. **Sila Genc:** Formal analysis, Investigation, Visualization, Writing - review & editing. **Jian Chen:** Formal analysis, Investigation, Writing - review & editing. **Joseph Y.M. Yang:** Formal analysis, Investigation, Writing - review & editing, Funding acquisition. **Chris Adamson:** Formal analysis, Investigation, Writing - review & editing. **Richard Beare:** Formal analysis, Investigation, Writing - review & editing. **Marc L. Seal:** Writing - review & editing, Resources, Funding acquisition. **Lex W. Doyle:** Conceptualization, Resources, Writing - review & editing, Supervision, Funding acquisition. **Jeanie LY. Cheong:** Conceptualization, Resources, Writing - review & editing, Supervision,





**Fig. 6.** Associations between neonatal global brain abnormality score and fixel-based analysis metrics.

The figures were generated by cropping the whole-brain template-derived tractogram so that it included only streamline segments that pass through fixels in which higher neonatal global brain abnormality scores were significantly associated with (A) lower fibre density (FD), fibre cross-section (FC) and fibre density and cross-section (FDC) at ages 7 and 13 years, and (B) less increase in FDC between ages 7 and 13 years, in the very preterm (VP) group ( $p < 0.05$ , family-wise error rate-corrected). Streamline segments were then coloured by direction (anterior-posterior = green; superior-inferior = blue; left-right = red). In (C), FDC values averaged across the significant fixels in (B) have been plotted against age, separately for VP children with normal/mild and moderate/severe neonatal global brain abnormality scores. In part A, all significant results presented were obtained from models adjusted for age and sex; for FC and FDC, there were no significant fixels after additionally adjusting for intracranial volume. In part B, all significant results presented were obtained from models adjusted for change in age, sex and change in intracranial volume.

**Funding acquisition.** Peter J. Anderson: Conceptualization, Resources, Writing - review & editing, Supervision, Funding acquisition.

### Acknowledgements

This research was conducted within the Victorian Infant Brain Study (VIBeS) and Developmental Imaging research groups, Murdoch Children's Research Institute and the Children's MRI Centre, the Royal Children's Hospital, Melbourne, Victoria. We thank members of the VIBeS and Developmental Imaging teams, the Royal Children's Hospital Medical Imaging staff for their assistance and expertise in the collection of the MRI data included in this study, and the children and families who participated.

This research was supported by the Australian National Health and Medical Research Council [NHMRC; Centre for Research Excellence 546519, 1060733 and 1153176; Project Grant 237117, 491209 and 1066555; Senior Research Fellowship 1081288 to PJA; Investigator Grant 1176077 to PJA; Career Development Fellowship 1085754 to DKT and 1141354 to JLYC, and; Early Career Fellowship 1012236 to DKT], the Murdoch Children's Research Institute, the Royal Children's Hospital, the Royal Children's Hospital Foundation [RCH1000 to JYMY], the Department of Paediatrics at the University of Melbourne, and the Victorian Government's Operational Infrastructure Support Program.

The funding organisations/sponsors had no role in the design and conduct of the study; collection, management, analysis, and interpretation of the data; preparation, review, or approval of the manuscript; and decision to submit the manuscript for publication. The authors have no potential conflicts of interest to disclose.

### Appendix A. Supplementary data

Supplementary data to this article can be found online at <https://doi.org/10.1016/j.neuroimage.2020.117068>.

### References

- Allin, M.P., Kontis, D., Walshe, M., et al., 2011. White matter and cognition in adults who were born preterm. *PLoS One* 6 (10), e24525.
- Andersson, J.L.R., Sotiropoulos, S.N., 2016. An integrated approach to correction for off-resonance effects and subject movement in diffusion MR imaging. *Neuroimage* 125, 1063–1078.
- Andersson, J.L., Skare, S., Ashburner, J., 2003. How to correct susceptibility distortions in spin-echo echo-planar images: application to diffusion tensor imaging. *Neuroimage* 20 (2), 870–888.
- Andersson, J.L.R., Graham, M.S., Zsoldos, E., Sotiropoulos, S.N., 2016. Incorporating outlier detection and replacement into a non-parametric framework for movement and distortion correction of diffusion MR images. *Neuroimage* 141, 556–572.
- Andersson, J.L.R., Graham, M.S., Drobnyak, I., Zhang, H., Filippini, N., Bastiani, M., 2017. Towards a comprehensive framework for movement and distortion correction of diffusion MR images: within volume movement. *Neuroimage* 152, 450–466.

- Barnett, M.L., Tumor, N., Ball, G., et al., 2018. Exploring the multiple-hit hypothesis of preterm white matter damage using diffusion MRI. *Neuroimage Clin* 17, 596–606.
- Bastiani, M., Cottaar, M., Fitzgibbon, S.P., et al., 2019. Automated quality control for within and between studies diffusion MRI data using a non-parametric framework for movement and distortion correction. *Neuroimage* 184, 801–812.
- Bhushan, C., Haldar, J.P., Joshi, A.A., Leahy, R.M., 2012. Correcting susceptibility-induced distortion in diffusion-weighted MRI using constrained nonrigid registration. In: 2012 Asia-Pacific Signal and Information Processing Association Annual Summit and Conference (Apsipa Asc). <Go to ISI>://WOS:000319456200258.
- Blencowe, H., Cousens, S., Oestergaard, M.Z., et al., 2012. National, regional, and worldwide estimates of preterm birth rates in the year 2010 with time trends since 1990 for selected countries: a systematic analysis and implications. *Lancet* 379 (9832), 2162–2172.
- Cole, T.J., Freeman, J.V., Preece, M.A., 1998. British 1990 growth reference centiles for weight, height, body mass index and head circumference fitted by maximum penalized likelihood. *Stat. Med.* 17 (4), 407–429.
- Constable, R.T., Ment, L.R., Vohr, B.R., et al., 2008. Prematurely born children demonstrate white matter microstructural differences at 12 years of age, relative to term control subjects: an investigation of group and gender effects. *Pediatrics* 121 (2), 306–316.
- Djamanakova, A., Faria, A.V., Hsu, J., et al., 2013. Diffeomorphic brain mapping based on T1-weighted images: improvement of registration accuracy by multichannel mapping. *J. Magn. Reson. Imag.* 37 (1), 76–84.
- Dubois, J., Hertz-Pannier, L., Cachia, A., Mangin, J.F., Le Bihan, D., Dehaene-Lambertz, G., 2009. Structural asymmetries in the infant language and sensori-motor networks. *Cerebr. Cortex* 19 (2), 414–423.
- Dubois, J., Dehaene-Lambertz, G., Kulikova, S., Poupon, C., Huppi, P.S., Hertz-Pannier, L., 2014. The early development of brain white matter: a review of imaging studies in fetuses, newborns and infants. *Neuroscience* 276, 48–71.
- Eikenes, L., Lohaugen, G.C., Brubakk, A.M., Skranes, J., Haberg, A.K., 2011. Young adults born preterm with very low birth weight demonstrate widespread white matter alterations on brain DTI. *Neuroimage* 54 (3), 1774–1785.
- Gajamange, S., Raffelt, D., Dhollander, T., et al., 2018. Fibre-specific white matter changes in multiple sclerosis patients with optic neuritis. *Neuroimage Clin* 17, 60–68.
- Geeraert, B.L., Lebel, R.M., Lebel, C., 2019. A multiparametric analysis of white matter maturation during late childhood and adolescence. *Hum. Brain Mapp.* 40 (15), 4345–4356.
- Genc, S., Malpas, C.B., Holland, S.K., Beare, R., Silk, T.J., 2017. Neurite density index is sensitive to age related differences in the developing brain. *Neuroimage* 148, 373–380.
- Genc, S., Seal, M.L., Dhollander, T., Malpas, C.B., Hazell, P., Silk, T.J., 2017. White matter alterations at pubertal onset. *Neuroimage* 156, 286–292.
- Genc, S., Smith, R.E., Malpas, C.B., et al., 2018. Development of white matter fibre density and morphology over childhood: a longitudinal fixel-based analysis. *Neuroimage* 183, 666–676.
- Genc, S., Malpas, C.B., Gulenc, A., et al., 2019. Longitudinal White Matter Development in Children Is Associated with Puberty, Attentional Difficulties, and Mental Health. *bioRxiv*. <https://doi.org/10.1101/607671>.
- Genc, S., Tax, C.M.W., Raven, E.P., Chamberland, M., Parker, G.D., Jones, D.K., 2020. Impact of b-value on estimates of apparent fibre density. *bioRxiv*. <https://doi.org/10.1101/2020.01.15.905802>.
- Hollund, I.M.H., Olsen, A., Skranes, J., et al., 2018. White matter alterations and their associations with motor function in young adults born preterm with very low birth weight. *Neuroimage Clin* 17, 241–250.
- Jeurissen, B., Leemans, A., Tournier, J.D., Jones, D.K., Sijbers, J., 2013. Investigating the prevalence of complex fiber configurations in white matter tissue with diffusion magnetic resonance imaging. *Hum. Brain Mapp.* 34 (11), 2747–2766.
- Jo, H.M., Cho, H.K., Jang, S.H., et al., 2012. A comparison of microstructural maturational changes of the corpus callosum in preterm and full-term children: a diffusion tensor imaging study. *Neuroradiology* 54 (9), 997–1005.
- Jones, D.K., Knosche, T.R., Turner, R., 2013. White matter integrity, fiber count, and other fallacies: the do's and don'ts of diffusion MRI. *Neuroimage* 73, 239–254.
- Kelly, C.E., Thompson, D.K., Chen, J., et al., 2016. Axon density and axon orientation dispersion in children born preterm. *Hum. Brain Mapp.* 37 (9), 3080–3102.
- Kidokoro, H., Neil, J.J., Inder, T.E., 2013. New MR imaging assessment tool to define brain abnormalities in very preterm infants at term. *Am. J. Neuroradiol.* 34 (11), 2208–2214.
- Kwon, S.H., Scheinost, D., Lacadie, C., et al., 2015. Adaptive mechanisms of developing brain: cerebral lateralization in the prematurely-born. *Neuroimage* 108, 144–150.
- Lebel, C., Beaulieu, C., 2011. Longitudinal development of human brain wiring continues from childhood into adulthood. *J. Neurosci.* 31 (30), 10937–10947.
- Leemans, A., Jones, D.K., 2009. The B-matrix must be rotated when correcting for subject motion in DTI data. *Magn. Reson. Med.* 61 (6), 1336–1349.
- Li, K., Sun, Z., Han, Y., Gao, L., Yuan, L., Zeng, D., 2015. Fractional anisotropy alterations in individuals born preterm: a diffusion tensor imaging meta-analysis. *Dev. Med. Child Neurol.* 57 (4), 328–338.
- Luders, E., Thompson, P.M., Toga, A.W., 2010. The development of the corpus callosum in the healthy human brain. *J. Neurosci.* 30 (33), 10985–10990.
- Malhotra, A., Sepehrizadeh, T., Dhollander, T., et al., 2019. Advanced MRI analysis to detect white matter brain injury in growth restricted newborn lambs. *Neuroimage Clin* 24, 101991.
- Mito, R., Raffelt, D., Dhollander, T., et al., 2018. Fibre-specific white matter reductions in Alzheimer's disease and mild cognitive impairment. *Brain* 141 (3), 888–902.
- Monson, B.B., Anderson, P.J., Matthews, L.G., et al., 2016. Examination of the pattern of growth of cerebral tissue volumes from hospital discharge to early childhood in very preterm infants. *JAMA Pediatr* 170 (8), 772–779.
- Oishi, K., Faria, A., van Zijl, P.C.M., Mori, S., 2011. MRI Atlas of Human White Matter, second ed. Elsevier B.V.
- Pandit, A.S., Ball, G., Edwards, A.D., Counsell, S.J., 2013. Diffusion magnetic resonance imaging in preterm brain injury. *Neuroradiology* 55 (Suppl. 2), 65–95.
- Pannek, K., Fripp, J., George, J.M., et al., 2018. Fixel-based analysis reveals alterations in brain microstructure and macrostructure of preterm-born infants at term equivalent age. *Neuroimage Clin* 18, 51–59.
- Papile, L.A., Burstein, J., Burstein, R., Koffler, H., 1978. Incidence and evolution of subependymal and intraventricular hemorrhage: a study of infants with birth weights less than 1,500 gm. *J. Pediatr.* 92 (4), 529–534.
- Pascoe, M.J., Melzer, T.R., Horwood, L.J., Woodward, L.J., Darlow, B.A., 2019. Altered grey matter volume, perfusion and white matter integrity in very low birthweight adults. *Neuroimage Clin* 22, 101780.
- Pecheva, D., Tournier, J.D., Pietsch, M., et al., 2019. Fixel-based analysis of the preterm brain: disentangling bundle-specific white matter microstructural and macrostructural changes in relation to clinical risk factors. *Neuroimage Clin* 23, 101820.
- Raffelt, D., Tournier, J.D., Fripp, J., Crozier, S., Connelly, A., Salvado, O., 2011. Symmetric diffeomorphic registration of fibre orientation distributions. *Neuroimage* 56 (3), 1171–1180.
- Raffelt, D., Tournier, J.D., Rose, S., et al., 2012. Apparent Fibre Density: a novel measure for the analysis of diffusion-weighted magnetic resonance images. *Neuroimage* 59 (4), 3976–3994.
- Raffelt, D.A., Smith, R.E., Ridgway, G.R., et al., 2015. Connectivity-based fixel enhancement: whole-brain statistical analysis of diffusion MRI measures in the presence of crossing fibres. *Neuroimage* 117, 40–55.
- Raffelt, D.A., Tournier, J.D., Smith, R.E., et al., 2017. Investigating white matter fibre density and morphology using fixel-based analysis. *Neuroimage* 144 (Pt A), 58–73.
- Rojas-Vite, G., Coronado-Leija, R., Narvaez-Delgado, O., et al., 2019. Histological validation of per-bundle water diffusion metrics within a region of fiber crossing following axonal degeneration. *Neuroimage* 201, 116013.
- Saigal, S., Doyle, L.W., 2008. An overview of mortality and sequelae of preterm birth from infancy to adulthood. *Lancet* 371 (9608), 261–269.
- Skranes, J., Vangberg, T.R., Kulseng, S., et al., 2007. Clinical findings and white matter abnormalities seen on diffusion tensor imaging in adolescents with very low birth weight. *Brain* 130 (Pt 3), 654–666.
- Smith, S.M., 2002. Fast robust automated brain extraction. *Hum. Brain Mapp.* 17 (3), 143–155.
- Smith, R.E., Tournier, J.D., Calamante, F., Connelly, A., 2013. SIFT: spherical-deconvolution informed filtering of tractograms. *Neuroimage* 67, 298–312.
- Thompson, D.K., Lee, K.J., van Bijnen, L., et al., 2015. Accelerated corpus callosum development in prematurity predicts improved outcome. *Hum. Brain Mapp.* 36 (10), 3733–3748.
- Tournier, J.D., Calamante, F., Connelly, A., 2007. Robust determination of the fibre orientation distribution in diffusion MRI: non-negativity constrained super-resolved spherical deconvolution. *Neuroimage* 35 (4), 1459–1472.
- Tournier, J.D., Calamante, F., Connelly, A., 2013. Determination of the appropriate b value and number of gradient directions for high-angular-resolution diffusion-weighted imaging. *NMR Biomed.* 26 (12), 1775–1786.
- Tournier, J.D., Smith, R., Raffelt, D., et al., 2019. MRtrix3: a fast, flexible and open software framework for medical image processing and visualisation. *Neuroimage* 202, 116137.
- Tustison, N.J., Avants, B.B., Cook, P.A., et al., 2010. N4ITK: improved N3 bias correction. *IEEE Trans. Med. Imag.* 29 (6), 1310–1320.
- Vangberg, T.R., Skranes, J., Dale, A.M., Martinussen, M., Brubakk, A.M., Haraldseth, O., 2006. Changes in white matter diffusion anisotropy in adolescents born prematurely. *Neuroimage* 32 (4), 1538–1548.
- Volpe, J.J., 2019. Dysmaturation of premature brain: importance, cellular mechanisms, and potential interventions. *Pediatr. Neurol.* 95, 42–66.
- Wood, N.S., Costeloe, K., Gibson, A.T., et al., 2005. The EPICure study: associations and antecedents of neurological and developmental disability at 30 months of age following extremely preterm birth. *Arch. Dis. Child. Fetal Neonatal Ed.* 90 (2), F134–F140.
- Young, J.M., Vandewouw, M.M., Mossad, S.I., et al., 2019. White matter microstructural differences identified using multi-shell diffusion imaging in six-year-old children born very preterm. *Neuroimage Clin* 23, 101855.